

Mathematical Model of Mouse Embryonic Cardiomyocyte Excitation–Contraction Coupling

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Excitation–contraction (E–C) coupling is the mechanism that connects the electrical excitation with cardiomyocyte contraction. Embryonic cardiomyocytes are not only capable of generating action potential (AP)-induced Ca^{2+} signals and contractions (E–C coupling), but they also can induce spontaneous pacemaking activity. The spontaneous activity originates from spontaneous Ca^{2+} releases from the sarcoplasmic reticulum (SR), which trigger APs via the $\text{Na}^+/\text{Ca}^{2+}$ exchanger (NCX). In the AP-driven mode, an external stimulus triggers an AP and activates voltage-activated Ca^{2+} intrusion to the cell. These complex and unique features of the embryonic cardiomyocyte pacemaking and E–C coupling have never been assessed with mathematical modeling. Here, we suggest a novel mathematical model explaining how both of these mechanisms can coexist in the same embryonic cardiomyocytes. In addition to experimentally characterized ion currents, the model includes novel heterogeneous cytosolic Ca^{2+} dynamics and oscillatory SR Ca^{2+} handling. The model reproduces faithfully the experimentally observed fundamental features of both E–C coupling and pacemaking. We further validate our model by simulating the effect of genetic modifications on the hyperpolarization-activated current, NCX, and the SR Ca^{2+} buffer protein calreticulin. In these simulations, the model produces a similar functional alteration to that observed previously in the genetically engineered mice, and thus provides mechanistic explanations for the cardiac phenotypes of these animals. In general, this study presents the first model explaining the underlying cellular mechanism for the origin and the regulation of the heartbeat in early embryonic cardiomyocytes.

INTRODUCTION

In this issue (see p. 397), we presented experimental characterization and central functional components of the excitation–contraction (E–C) coupling and pacemaking of embryonic (E9–E11) mouse ventricular cardiomyocytes (Rapila et al., 2008). According to the experiments, these cells are capable of maintaining their activity alone by producing spontaneous cytosolic calcium oscillations upon repetitive calcium releases from the SR as suggested earlier (Sasse et al., 2007). The same cells are also capable of producing action potential (AP)-induced calcium influx and subsequent CICR from the SR upon electrical stimulation. In the developing heart, the APs triggered could conduct from cell to cell, thereby synchronizing the electrical activity and contraction of adjacent cells. In addition to this, we identified the mechanisms behind the spontaneous activity of the SR release. We showed that these calcium oscillations require functional ryanodine receptors (RyRs), inositol-3-phosphate receptors (IP_3Rs), and SR Ca^{2+} ATPase (SERCA) (Rapila et al., 2008). Further, we showed that the frequency of the spontaneous oscillations depends on the calcium leak through the IP_3Rs , which provides a mechanism for the regu-

lation of the heart rate of the embryonic heart. Collectively, the detailed experimental characterization of the individual features of E–C coupling and pacemaking in E9–E11 myocytes introduces a view of a rather complicated array of cellular functions. Therefore, to further analyze how these different mechanisms operate in parallel, we built a mathematical model into which we incorporated the experimentally characterized components of calcium signaling and excitability of these cells. Mathematical modeling has been widely used as a tool in explaining and studying E–C coupling in adult cardiomyocytes (Luo and Rudy, 1994; Dokos et al., 1996; Jafri et al., 1998; Pandit et al., 2001; Bondarenko et al., 2004). However, based on our results, the differences between embryonic and adult cardiomyocytes are so dramatic that novel approaches are required to model the embryonic cardiomyocyte E–C coupling and pacemaking. In embryonic cardiomyocytes, the cytosolic Ca^{2+} signals are more heterogeneous than in adult cardiomyocytes (Rapila et al., 2008). Therefore, instead of the common pool approach used in the adult myocyte models (Luo and Rudy, 1994; Dokos et al., 1996; Jafri et al., 1998; Pandit et al., 2001; Bondarenko et al., 2004), a more detailed description of the cytosolic Ca^{2+} dynamics was required. In addition, the SRs in adult models (Luo and Rudy,

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Abbreviations used in this paper: AP, action potential; E–C, excitation–contraction; I_{CaL} , L-type Ca^{2+} current; I_{CaT} , T-type Ca^{2+} current; I_{h} , hyperpolarization-activated current; I_{K1} , time-independent background K^+ current; I_{KDR} , slowly activated delayed rectifier K^+ current; I_{Na} , fast Na^+ current; IP_3R , inositol-3-phosphate receptor; NCX, $\text{Na}^+/\text{Ca}^{2+}$ exchanger; r.p., resting potential; RyR, ryanodine receptor; SERCA, SR Ca^{2+} ATPase; SL, sarcolemmal.

The online version of this article contains supplemental material.

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1994; Dokos et al., 1996; Jafri et al., 1998; Pandit et al., 2001; Bondarenko et al., 2004) produce only calcium-triggered, nonspontaneous Ca^{2+} releases. Spontaneous SR and ER Ca^{2+} oscillations, such as those triggering the activity of the embryonic cardiomyocytes, have been described and modeled in a variety of other cell types (Deyoung and Keizer, 1992; Keizer and Levine, 1996; Sneyd et al., 2003), but not in cardiomyocytes. Therefore, to model the E9-E11 cardiomyocyte E–C coupling and pacemaking, this type of SR dynamics had to be introduced to the model.

Here, we present a model of E–C coupling and pacemaking in E9-E11 mouse ventricular cardiomyocytes with the novel features described above. For developing the model, we also characterized the major ion currents in the sarcolemmal (SL) membrane of E9-E11 cardiomyocytes. The model is constructed based on this electrophysiological data and data from our accompanying paper (Rapila et al., 2008). We use the model to study if the identified SL ion currents and the SR components (IP_3R , RyR , and SERCA) are sufficient to explain the function of E9-E11 cardiomyocytes. With the model we show the following: (1) IP_3R , RyR , and SERCA , with obligatory roles for all, can produce spontaneous cytosolic Ca^{2+} oscillations at the rate of ~ 0.2 – 1.1 Hz; and (2) the identified SL ion currents together compose an excitable membrane that (a) produces APs when cytosolic Ca^{2+} oscillates spontaneously, (b) produces APs and CICRs when exposed to external electrical excitation, and (c) is quiescent without either of these stimuli. We further simulate the model with modified hyperpolarization-activated current (I_f), $\text{Na}^+/\text{Ca}^{2+}$ exchanger (NCX), and SR Ca^{2+} buffer calreticulin amounts and show that our simulations are in line with previous experimental studies with corresponding transgenic animals (Mesaali et al., 1999; Wakimoto et al., 2000; Nakamura et al., 2001; Stieber et al., 2003). These simulations validate our model further and also provide the underlying mechanism for the observed E–C coupling and pacemaking alterations in these transgenic animals.

MATERIALS AND METHODS

Electrophysiological Recordings

The cell isolation and culturing and the electrophysiological recordings were performed as described in this issue in Rapila et al. (2008). The used solutions and recording methods are summarized in Table S1, which is available at <http://www.jgp.org/cgi/content/full/jgp.200809961/DC1>. Ion currents were measured at $+25^\circ\text{C}$. The membrane currents were scaled by dividing them with the measured cell membrane capacitance.

Mathematical Model of the Embryonic Ventricular Myocyte

A mathematical model of the E9-E11 embryonic mouse ventricular myocyte was developed and simulated. The model describes the function of SR and SL ion channels, membrane voltage dynamics, and cytosolic Ca^{2+} , Na^+ and K^+ , and SR Ca^{2+} concentration dynamics. A fundamental feature of the model is that in

addition to a time coordinate, the cytosolic Ca^{2+} concentration is also modeled as a function of a spatial coordinate. All parameters of the components and the environmental parameters of the model were fitted to our own experimental data and experimental conditions (in this and in Rapila et al. [2008]) whenever possible and necessary. Complete model equations are shown in the Supplemental text, which is available at <http://www.jgp.org/cgi/content/full/jgp.200809961/DC1>.

Structure of the Model. As shown in Fig. 1, the cell and the intracellular structures were assumed to have spherical shapes. The nucleus is located in the center of the cell and the SR on the surface of the nucleus, and the cytosol is the space between the SL and SR. The dimensions of the structure were estimated from our confocal and light microscope images and from patch-clamp data by calculating the membrane area and r_{cell} from the membrane capacitance (Table S2, available at <http://www.jgp.org/cgi/content/full/jgp.200809961/DC1>).

Ca^{2+} Diffusion and Buffering in Cytosol. The spatial differences of the Ca^{2+} concentration within the cytosol were modeled using Fick's law of diffusion. For the calcium diffusion coefficient D_{Ca} of the model, we used the value previously reported for calcium in water, $0.79 \mu\text{m}^2/\text{ms}$ (Cussler, 1997) (Table S5, available at <http://www.jgp.org/cgi/content/full/jgp.200809961/DC1>). With this D_{Ca} value, the model reproduced well the delay in Ca^{2+} signal between cytosol areas below the SR and SL, which was experimentally defined by Rapila et al. (2008) (28.5 ± 4.9 ms; $n = 12$). Due to the shape of the model cell, the diffusion is modeled using spherical coordinates and by assuming radial symmetry. The cytosolic Ca^{2+} buffering of troponin C and calmodulin is modeled as described previously (Luo and Rudy, 1994). The free and buffered Ca^{2+} concentrations are calculated for all radii values between boundaries. Embryonic myocytes have a lower Ca^{2+} binding capacity than adult myocytes, which is mostly caused by a lower troponin C concentration (Creazzo et al., 2004). Based on this, we reduced the amount of troponin C to 30% and calmodulin to 75% of the original values.

SL Ion Channels. The models of the NCX (Luo and Rudy, 1994), I_f (Pandit et al., 2001), fast Na^+ current (I_{Na}) (Bondarenko et al., 2004), slowly activated delayed rectifier K^+ current (I_{KDR}) (Dokos et al., 1996), time-independent background K^+ current (I_{K1}) (Dokos et al., 1996), L-type Ca^{2+} current (I_{CaL}) (Bondarenko et al., 2004), and T-type Ca^{2+} current (I_{CaT}) (Dokos et al., 1996) were fitted to our whole cell voltage-clamp data (Fig. 2). The fitted conductances were scaled from $T = 25^\circ\text{C}$ (in Fig. 2) to $T = 34^\circ\text{C}$ with $Q_{10} = 1.35$ (Hart, 1983; Hille, 2001), except $Q_{10\text{-NCX}} = 1.6$ (Debetto et al., 1990; Puglisi et al., 1996; Shannon et al., 2004) and $Q_{10\text{-ICaL}} = 1.8$ (Puglisi et al., 1999; Shannon et al., 2004). The I_f time constant was scaled with $Q_{10} = 3$ (Hart, 1983; Hille, 2001). As described previously, the fitting of the I_{Na} was based partly on the AP upstroke properties (Bondarenko et al., 2004). The background Ca^{2+} current is modeled as a linear ohmic current and fitted to obtain a physiologically correct diastolic $[\text{Ca}^{2+}]$ (~ 0.1 – $0.2 \mu\text{M}$). The model of the NaK-ATPase (Luo and Rudy, 1994) was fitted to maintain physiologically correct intracellular Na^+ and K^+ concentrations (~ 14 and ~ 140 mM, respectively). The ion currents change the cytosolic $[\text{Ca}^{2+}]$ below the SL and the cytosolic common pool $[\text{Na}^+]$ and $[\text{K}^+]$.

SR. SR is modeled as a common pool compartment for Ca^{2+} ions. In the SR the Ca^{2+} is buffered with calreticulin using a similar buffering model as in the cytosol. Ca^{2+} ions move from the SR to the cytosol via RyR and IP_3R and from the cytosol to SR via SERCA . The models of these channels and the Ca^{2+} flux via these channels interact with the cytosolic $[\text{Ca}^{2+}]$ below the SR ($[\text{Ca}^{2+}]_{\text{subSR}}$). The function of RyR is modeled using a previously published model

(Keizer and Levine, 1996). The function of IP_3R is modeled using a model that takes the $[\text{IP}_3]$ as an input parameter and computes the IP_3R Ca^{2+} flux based on the open (O) and active (A) states of the receptor (Sneyd and Dufour, 2002). The results presented here were simulated using $[\text{IP}_3] = 0.075 \mu\text{M}$ unless stated otherwise. The model of SERCA (Jafri et al., 1998) is used with half-maximal activation by $[\text{Ca}^{2+}]_{\text{subSR}}$ set to $0.25 \mu\text{M}$ (Frank et al., 2000).

The values for calreticulin concentration, amounts of SR ion channels, and $[\text{IP}_3]$ were fitted to give a physiologically relevant $[\text{Ca}^{2+}]$ transient amplitude, a fractional release comparable to our measurements, and spontaneous Ca^{2+} oscillation frequencies that are comparable to the experimentally observed range of oscillation frequencies (0.1–1.3 Hz; Rapila et al. [2008]).

Simulation Methods. The model consists of 31 ordinary differential equations combined with one partial differential equation. The model was simulated in the Matlab 6.5 (The Mathworks) environment using a self-written solver algorithm for combined partial and ordinary differential equation systems based on the forward Euler method (Korhonen and Tavi, 2008). We used a spatial step size of $\Delta r = 0.1 \mu\text{m}$ and time step sizes of $\Delta t = 1\text{--}0.00001$ ms to obtain solutions with a relative error of $<0.1\%$ at each integration step. The simulations shown here were started from the steady-state initial conditions. The steady-state conditions were obtained by simulating the model until the intracellular ion concentrations were stable. The electrical stimulation of the model cell was simulated by applying a stimulus current of -80 pA/pF (-120 pA/pF in Fig. 5) for 0.5 ms. In some simulations, the models of individual ion channels were driven with a voltage-clamp protocol. The effect of caffeine was simulated by setting the diffusion rate of RyR Ca^{2+} flux to a large constant value (see Supplemental text). The SERCA Ca^{2+} flux was set to zero, as the Ca^{2+} is extruded almost completely with SL mechanisms when caffeine is applied to cardiomyocytes (Bers, 2001). The effect of $\text{IP}_3\text{-AM}$ seen in experiments was simulated by increasing the $[\text{IP}_3]$ slowly ($10^{-3} \mu\text{M/s}$) as the de-esterification of $\text{IP}_3\text{-AM}$ to IP_3 in cytosol is not instant.

Data Analysis

Data analysis was made using the Clampfit 9.2 (MDS Analytical Technologies), Origin 7.5 (OriginLab Corporation), and Matlab 6.5 (The Mathworks) software. Clampfit's leak resistance subtraction and software filters were used when necessary.

Matlab's (The Mathworks) "nlinfit" function for nonlinear least-squares data fitting by the Gauss-Newton method was used to fit the model components to experimental data. Results are expressed as mean \pm SEM.

Online Supplemental Material

The online supplemental material includes a table for the used solutions and recording methods in electrophysiological recordings (Table S1), the parameters of the model (Tables S2–S5), complete model equations (Supplemental text), a figure of the simulated effects of RyR, IP_3R , and SERCA blocks (Fig. S1), and an animation of the simulated spontaneous activity (Video 1). The online supplemental material is available at <http://www.jgp.org/cgi/content/full/jgp.200809961/DC1>.

RESULTS

Electrophysiological Characterization of the Mouse E9-E11 Ventricular Myocytes

We identified seven major ion current types from E9-E11 mouse ventricular cardiomyocytes (Fig. 2). The I_{NCX} mea-

sured as the Ni^{2+} -sensitive current had a density of $-0.55 \pm 0.19 \text{ pA/pF}$ ($n = 7$) at -100 mV . The theoretical reversal potential for I_{NCX} in the recording solution ($3E_{\text{Na}} - 2E_{\text{Ca}} = -15 \text{ mV}$) (Despa et al., 2003) agrees with the reversal potential in our experimental I-V relation for I_{NCX} ($\sim -12 \text{ mV}$, Fig. 2 A). As described previously (Yasui et al., 2001), we found an I_f current, which activates slowly ($\tau \sim 0.3\text{--}3 \text{ s}$) upon hyperpolarization of the cell membrane. The threshold for the activation of I_f was $\sim -70 \text{ mV}$ (Fig. 2 B). The recorded I_{Na} current had a similar I-V relation shape, as described previously (Doevendans et al., 2000) (Fig. 2 C), and had a large peak current of $-92.1 \pm 13.8 \text{ pA/pF}$ at -20 mV ($n = 11$). We identified two types of repolarizing K^+ currents: an I_{KDR} and an I_{K1} (Fig. 2 D). The I_{KDR} is active at V_m above -30 mV , and it corresponds to the early repolarization of the AP. The I_{K1} operates at smaller V_m values and contributes to the late repolarization of the AP and to the resting potential (r.p.). Both L- and T-type voltage-activated Ca^{2+} channels are present in embryonic mouse cardiomyocytes (Seisenberger et al., 2000; Cribbs et al., 2001). We recorded the I_{CaL} with a peak amplitude of $-4.5 \pm 0.6 \text{ pA/pF}$ ($n = 11$) and I_{CaT} with a peak amplitude of $-0.59 \pm 0.21 \text{ pA/pF}$ ($n = 5$) (Fig. 2 E). We included all of these seven types of ion channels in the model with similar voltage-dependent behavior as recorded in our experiments (Fig. 2). In addition to these currents, the NaK-ATPase and background Ca^{2+} leak were included in the SL membrane (Fig. 1).

Simulation of the Pacemaking and E-C Coupling of an E9-E11 Cardiomyocyte

In Rapila et al. (2008) in this issue, we showed that the spontaneous Ca^{2+} signals in E9-E11 cardiomyocytes

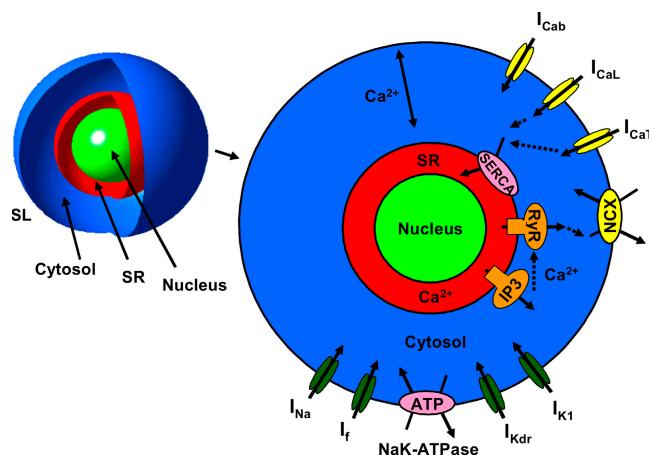


Figure 1. A schematic diagram of the mathematical model of the mouse early embryonic (E9-E11) cardiomyocyte. The SL components are background Ca^{2+} current (I_{Cab}), I_{CaL} , I_{CaT} , NCX , I_{K1} , I_{KDR} , NaK-ATPase, I_f , and I_{Na} . The SR components are Ca^{2+} pump (SERCA), RyR, and IP_3R . Ca^{2+} diffuses radially in the cytosol and is buffered to troponin and calmodulin in cytosol and to calreticulin in the SR. The model also includes dynamic cytosol Na^+ and K^+ concentrations. The compartments are not in scale.

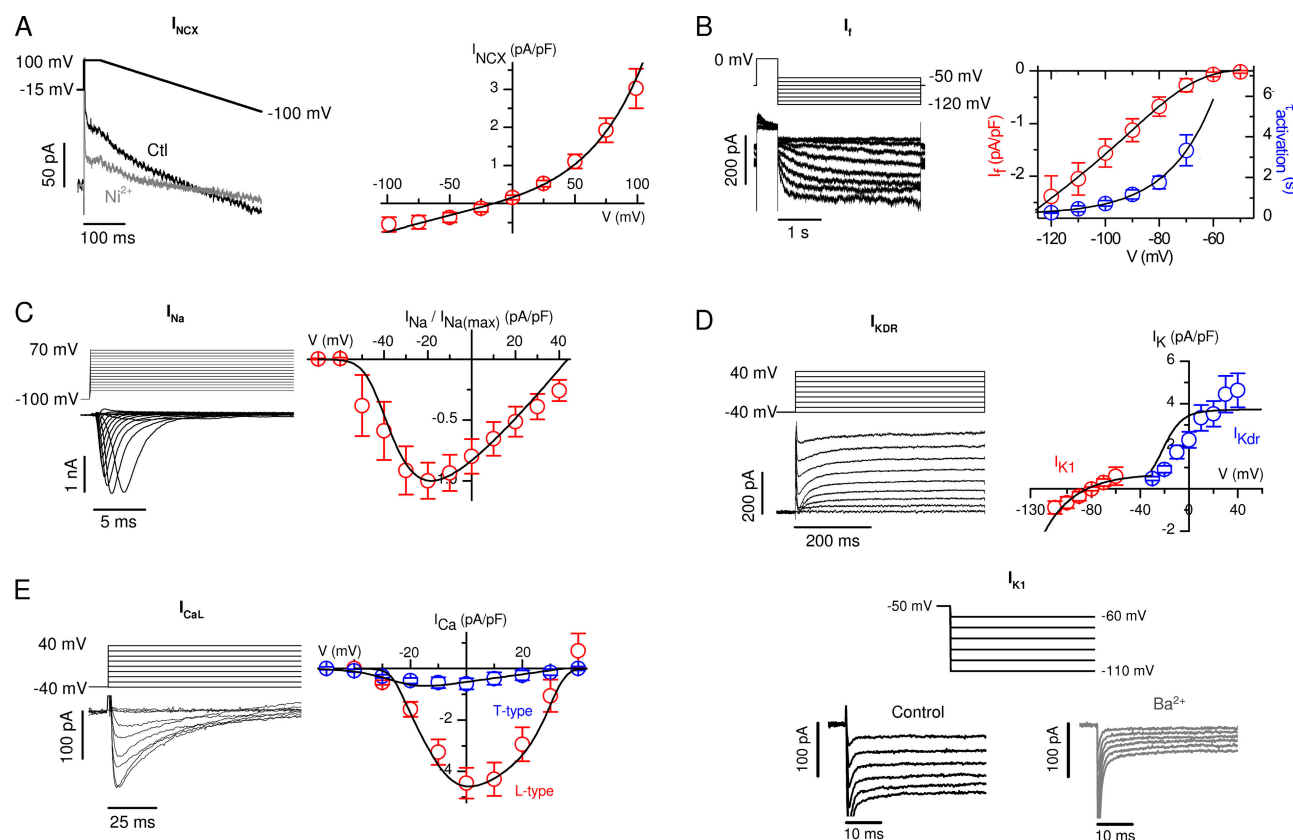


Figure 2. The current–voltage relations of the ion currents in the E9–E11 mouse cardiomyocytes and in the mathematical model. (A) I_{NCX} , (B) I_f (the activation time constant is also shown), (C) I_{Na} , (D) I_{K1} and I_{KDR} , and (E) T- and L-type calcium channels (top right panel). In each case, red or blue symbols denote the experimentally defined features of the ion currents that were adopted into the model (black solid lines). The representative recordings are shown in the left column of each panel.

require both IP_3R and RyR at the SR. We suggested that the Ca^{2+} leak via IP_3R increases the cytosolic Ca^{2+} and triggers the Ca^{2+} release from RyR . In 48–72-h cultured early embryonic cardiomyocytes (Sasse et al., 2007) and in stem cell–derived differentiating cardiomyocytes (Mery et al., 2005), IP_3Rs are able to produce $[Ca^{2+}]_i$ oscillations alone. These kind of oscillations have been modeled before, and they require either biphasic (activation/inactivation) calcium-dependent modulation of IP_3R (Atri et al., 1993) or oscillation of cytosolic $[IP_3]$ (Politi et al., 2006). Sensitivity to $[IP_3]$ is common to all IP_3R isoforms (Ramos-Franco et al., 1998; Hagar and Ehrlich, 2000), whereas calcium-dependent inactivation is characteristic to IP_3R -type 1 only (Hagar et al., 1998; Ramos-Franco et al., 1998). In our experiments (Rapila et al., 2008), IP_3R activation alone did not produce spontaneous Ca^{2+} oscillations. Activation of IP_3Rs produced only an $[IP_3]$ -dependent constant Ca^{2+} leak. Consequently, IP_3Rs have no Ca^{2+} -dependent inactivation with increasing $[Ca^{2+}]_i$. Because these calcium activation features are characteristic of the type 2 IP_3R (Ramos-Franco et al., 1998), the predominant IP_3R isoform in ventricular myocytes (Perez et al., 1997), we implemented a model of the type 2 IP_3R (Sneyd and Dufour,

2002) to the SR of our mathematical model. Together with modeled $RyRs$ (Keizer and Levine, 1996) and IP_3Rs in the simulation of our model with no external stimulus, the model produces spontaneous activity that is initiated by a slowly increasing Ca^{2+} leak via IP_3R from SR to cytosol (Fig. 3, A and B, and Video 1, which is available at <http://www.jgp.org/cgi/content/full/jgp.200809961/DC1>). When a certain threshold in cytosolic $[Ca^{2+}]$ near the SR is crossed, the $RyRs$ are triggered and a large Ca^{2+} release occurs from the SR to the cytosol. Altogether, the simulated RyR and IP_3R channels have quite different dynamic features; $RyRs$ produce rapid transient openings, whereas the IP_3R open probability changes slowly and remains almost constant in the time scale of the pacemaking cycle (Fig. 3 B and Video 1).

The SR Ca^{2+} release and NCX have been shown to play a role in embryonic pacemaking (Sasse et al., 2007) and adult pacemaker cells (Bogdanov et al., 2001; Vinogradova et al., 2005). In our accompanying paper in this issue, we showed that the spontaneously released Ca^{2+} diffuses in the cytosol from SR to SL, where it triggers an AP (Rapila et al., 2008). The triggering of the AP was shown to depend on the I_{NCX} . E9–E11 cardiomyocytes have a relatively

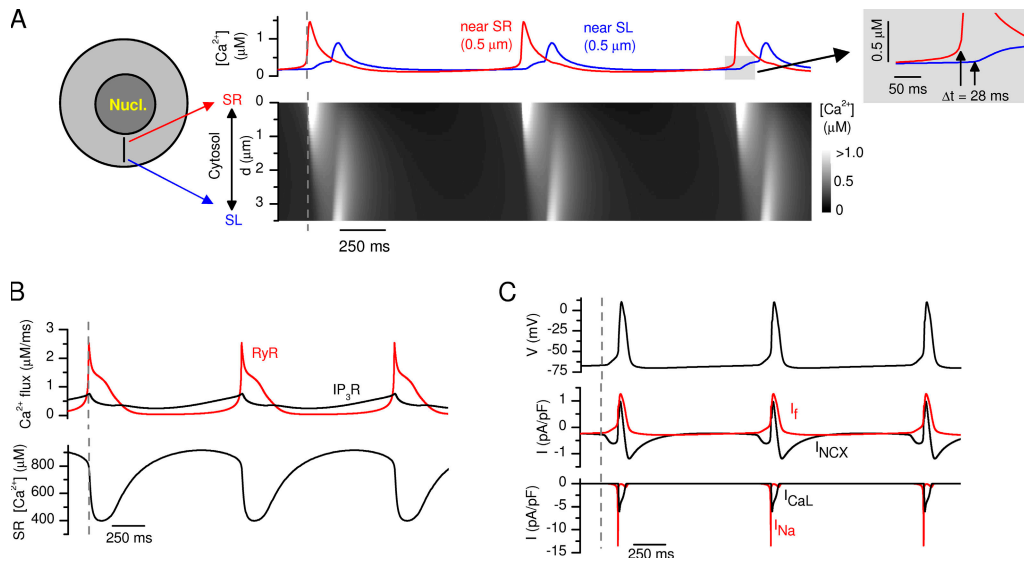


Figure 3. Simulated cardiomyocyte spontaneous activity. (A) Near-SR and near-SL Ca^{2+} concentrations (top panel) from the simulated cytosolic calcium distribution (bottom panel). (B) The corresponding calcium fluxes through RyRs and IP₃Rs and the SR Ca^{2+} concentration. (C) The corresponding APs accompanied by central ion currents: I_f with I_{NCX} and I_{CaL} with I_{Na} .

long diffusion distance from SR to SL, which is implemented into the model. Long distance results in a time delay between the near-SR and near-SL Ca^{2+} increment during simulated spontaneous SR Ca^{2+} release and cytosolic Ca^{2+} diffusion (Fig. 3 A and Video 1). The increment of the near-SL Ca^{2+} activates a depolarizing I_{NCX} current when NCX extrudes Ca^{2+} (Fig. 3 C and Video 1). The V_m depolarizes slowly until the threshold for I_{Na} activation is crossed and the AP is initiated. The activated I_{Na} causes rapid depolarization of the cell membrane and subsequently also activates the voltage-activated Ca^{2+} channels, I_{CaL} and I_{CaT} (Fig. 3 C and Video 1).

Even though the E9-E11 cardiomyocytes are capable of producing their cytosolic Ca^{2+} transients and subsequent APs spontaneously, the activity can also be synchronized with an external stimulus (Rapila et al., 2008). The cells can thus maintain their activity alone but also synchronize their activity with other cells to form coordinated contraction. In line with the experiments, the simulations showed that the pacemaking and E–C coupling mode can coexist in the same cell. We simulated the effect of an external electrical excitation during spontaneous activity of the model cell. The membrane voltage and intracellular Ca^{2+} oscillations were synchronized to the frequency of the stimulus, and the intracellular Ca^{2+} gradients were reversed compared with the spontaneous activity (Fig. 4 A). During external pacing, the Ca^{2+} increases first at the SL side when AP-activated Ca^{2+} intrudes to the cytosol (Fig. 4 A). This Ca^{2+} diffuses through the cytosol to the sub-SR region and activates CICR via RyR. The overlay of the I_{NCX} during spontaneous and externally evoked activity reveals a depolarizing “hump” in the I_{NCX} curve that activates the AP during spontaneous Ca^{2+} oscillations, but which is

naturally not present in the I_{NCX} curve during external pacing (Fig. 4 B).

The difference between spontaneous and paced activity can also be seen from the net SL and SR fluxes (Fig. 4 C). This naturally results from the fact that during the spontaneous activity, the Ca^{2+} is first released from the SR side, whereas during the paced activity the Ca^{2+} release occurs first at the SL side. The released amounts of Ca^{2+} from both sides of the cytosol are taken up during relaxation. This produces net integrals of zero for the SR and SL Ca^{2+} fluxes over one cycle of activity, and thus the Ca^{2+} homeostasis is maintained in the model (Fig. 4 C). During spontaneous activity, the net SL Ca^{2+} flux extrudes 1.1 μM of Ca^{2+} when NCX triggers the AP. The voltage-activated Ca^{2+} channels I_{CaL} along with the minor contribution of I_{CaT} , I_{CaB} , and I_{NCX} reverse mode (Ca^{2+} intrusion mode) together provide sufficient Ca^{2+} intrusion, compensating for the Ca^{2+} extrusion by NCX during activation of the AP. This compensation prevents the depletion of SR Ca^{2+} and cessation of the spontaneous activity in E9-E11 cardiomyocytes as we described in Rapila et al. (2008).

Simulations with our model produce $[\text{Ca}^{2+}]_i$, $[\text{Na}^+]_i$, and $[\text{K}^+]_i$ values that are physiologically coherent (Table I) (Bers, 2001), and the r.p. and AP amplitude values are also comparable to experimental data (Table I) (Rapila et al., 2008). In the experiments, we also estimated the fractional Ca^{2+} release by comparing the amplitude of the twitch Ca^{2+} transient, which equals the sum of calcium fluxes from the SR and the SL to cytosol, to the amplitude of the caffeine-induced Ca^{2+} transient, which represents the whole SR Ca^{2+} content. By comparing the twitch Ca^{2+} transient to the caffeine-induced transient, it was calculated that during a spontaneous calcium

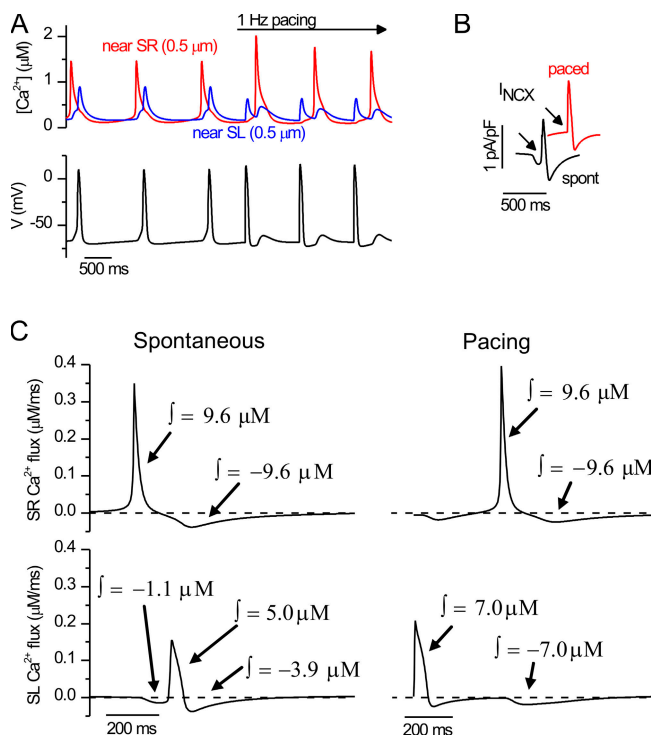


Figure 4. Calcium fluxes during spontaneous and stimulated activity. (A) Simulated spontaneous APs followed by simulated electrically evoked APs (bottom) with corresponding near-SR and near-SL calcium signals (top). (B) The difference in the I_{NCX} during spontaneous and electrically evoked activity. Arrows show the prominent inward current during spontaneous activity, which is absent during electrically evoked APs. (C) The net Ca^{2+} fluxes from the SR to cytosol (top) and from the extracellular space to cytosol (bottom). The left column shows the fluxes during spontaneous activity, and the right column shows them during the electrically evoked activity. The integrals of the positive and negative phases are indicated with arrows. The concentrations are in the volume of the cytosol.

transient, the SR and SL sources produce Ca^{2+} intrusion, which is $56.5 \pm 0.5\%$ compared with the total SR Ca^{2+} content (Rapila et al., 2008). The corresponding simulated value for Ca^{2+} intrusion from SL and SR sources versus SR Ca^{2+} content during activation of spontaneous twitch is 70% (Table I and Fig. 4 C).

It has been reported that embryonic cardiomyocytes have a smaller cytosolic Ca^{2+} buffering capacity per cytosol volume than adult cardiomyocytes (Creazzo et al., 2004). Taking this into account in the model, smaller Ca^{2+} cycling per cytosol volume between the cytosol and Ca^{2+} sources (SR and the extracellular space) is required to produce contraction and relaxation. In the embryonic cardiomyocyte, the amount of cycled Ca^{2+} (i.e., the net Ca^{2+} release to cytosol) during a spontaneous twitch in cytosol volume is $9.6 - 1.1 + 5.0 = 13.5 \mu M$ (Fig. 4 C), which is 35% of that in the adult mouse ventricular myocyte ($39 \pm 3 \mu M$) (Maier et al., 2003). Furthermore, the diastolic SR Ca^{2+} content in cytosol volume in the spontaneously beating embryonic cardiomyocyte is $19.3 \mu M$

TABLE I
Parameters of the Simulation Results

Simulated parameter	Spontaneous	Pacing
$[Na^+]_i$ diastolic (mM)	13.5	13.8
$[K^+]_i$ diastolic (mM)	142.4	142.2
r.p. mean (mV)	-68.5	-68.3
AP amplitude (mV)	78.7	82.9
$[Ca^{2+}]_i$ diastolic (μM)		
Near SL (0.5 μm)	0.17	0.19
Near SR (0.5 μm)	0.12	0.10
Ca^{2+} transient amplitude (μM)		
Near SL (0.5 μm)	0.73	0.46
Near SR (0.5 μm)	1.4	1.6
SR Ca^{2+} content in cytosol volume (μM)	19.3	16.9

(Table I), which is $\sim 14\%$ of that in the adult mouse ventricular myocyte ($142 \pm 9 \mu M$) (Maier et al., 2003). To make a reasonable comparison, the Ca^{2+} concentrations above are in the cytosol volume of the corresponding cell type to normalize the effect of different cell size between adult and embryonic cardiomyocytes.

The mode for spontaneous Ca^{2+} oscillations and the mode for AP-induced Ca^{2+} transients can be separated on the basis of their resting potential boundaries. We simulated the spontaneous and externally paced activity of the model cell while adjusting the membrane voltage with constant current injection. We found that spontaneous calcium release can operate at relatively depolarized membrane potentials between -88 to -27 mV, whereas AP-induced CICR is recruited between -107 to -38 mV (Fig. 5). The spontaneous activity cannot operate at r.p. values below -88 mV because hyperpolarization increases Ca^{2+} extrusion via NCX and thereby depletes the SR Ca^{2+} content. On the other hand, the externally triggered AP-driven mode cannot operate at r.p. values above -38 mV because depolarization inactivates the voltage-activated Ca^{2+} channels in the SL. Below -70 mV, 1 Hz pacing is not possible because longer diastole is required to refill the SR due to the higher Ca^{2+} extrusion via NCX. On the other hand, above -70 mV the cell cannot be synchronized to pacing frequencies 0.25 and 0.5 Hz because the frequency of the spontaneous activity is higher. This is in line with our suggestion (Rapila et al., 2008) that the activity in tissue is synchronized to the cell with the highest frequency.

The spontaneous Ca^{2+} and V_m activities of the E9-E11 mouse cardiomyocytes rely on the cytosolic Ca^{2+} oscillations originating from the SR (Rapila et al., 2008). Similarly in our model, the inhibition of RyR stopped the spontaneous Ca^{2+} oscillations and APs (Fig. 6 A). Also in line with experimental results (Rapila et al., 2008), the model cell without functional RyRs was still able to produce SL-originated Ca^{2+} signals and APs with external pacing (Fig. 6 B). The amplitude of these Ca^{2+} signals was reduced when the RyRs were inhibited in simulation

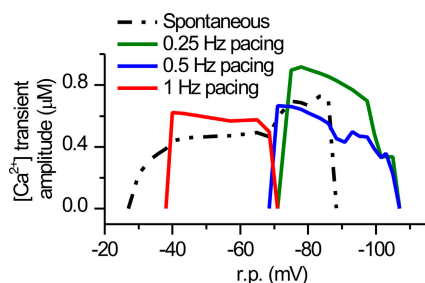


Figure 5. The resting potential windows favoring spontaneous Ca^{2+} activity and Ca^{2+} activity generated by electrical pacing. A constant current from 4 to -2.5 pA/pF with 0.25 pA/pF intervals was applied to the model cell to adjust the r.p. of the model cell to values between -107 and -27 mV. At each r.p. value, the spontaneous and paced (0.25, 0.5, and 1 Hz) cytosolic Ca^{2+} activity was observed for 10 s after 40 s of stabilization of the model. The figure shows the average amplitudes spontaneously evoked and electrically stimulated cytosolic $[\text{Ca}^{2+}]$ transients at given frequency.

and experiments (Rapila et al., 2008) to 42.3 versus $32.5 \pm 2.3\%$ (average cytosolic Ca^{2+} transient), respectively, as no CICR occurred. Just like in the experiments (Rapila et al., 2008), the block of either SERCA or IP_3R both stopped the spontaneous activity while the electrical excitability was maintained (Fig. S1, available at <http://www.jgip.org/cgi/content/full/jgip.200809961/DC1>). Based on these simulations, the ion current types and densities recorded from E9-E11 myocytes (Fig. 2) are incapable of producing V_m oscillations without an intracellular Ca^{2+} stimulus or external electrical excitation. For spontaneous Ca^{2+} oscillations, all three SR Ca^{2+} handling components are required. Without SERCA the SR Ca^{2+} stores are depleted, without RyRs the IP_3Rs cannot produce transient Ca^{2+} signals, and without IP_3Rs the RyRs are not activated without a sufficient cytosolic Ca^{2+} trigger.

To further validate the function of the SR and the dynamics of RyRs and IP_3Rs , we simulated the cytosolic Ca^{2+} under pharmacological stimulation of these receptors as in our experiments (Rapila et al., 2008). In the presence of IP_3R block, the simulated effect of caffeine, which rapidly opens the RyRs, produces a rapidly activating large Ca^{2+} transient (Fig. 7 A). The amplitudes of the sub-SR and sub-SL caffeine-induced Ca^{2+} transients are ~ 1.5 -fold compared with normal spontaneous Ca^{2+}

transients. In contrast to this, the simulated effect of the applied $\text{IP}_3\text{-AM}$ stimulating the IP_3R with RyR block produces only an increasing Ca^{2+} leak via IP_3R , which slowly increases the diastolic $[\text{Ca}^{2+}]_i$ (Fig. 7 B). Both of these simulations are in line with our experiments (Rapila et al., 2008) and with our previous conclusions that the RyR is the only possible route for transient Ca^{2+} release in these cells, but the IP_3R plays a role as a stimulator of RyR.

To support our conclusion that IP_3R Ca^{2+} leak stimulates RyR openings, we showed that stimulation of IP_3Rs with $\text{IP}_3\text{-AM}$ increases the frequency of spontaneous activity (Rapila et al., 2008). This same regulatory mechanism is reproduced in our model (Fig. 7 C). In the simulations, the oscillation frequency showed sigmoidal dependence on the $[\text{IP}_3]$. The possible oscillation frequencies achieved with $[\text{IP}_3]$ regulation in the model cell were in the range of ~ 0.2 to 1.1 Hz. In the experiments (Rapila et al., 2008), the frequencies of the spontaneous activities (global cytosolic Ca^{2+} transients and APs) were all within the range of 0.1 to 1.3 Hz (Fig. 7 D). This supports the idea that the dynamics and the structure of SR in the model are comparable to those in real E9-E11 cardiomyocytes. Modeling also supports the conclusions drawn from the experiments and demonstrates that in theory $[\text{IP}_3]$ could act as a major regulator of the embryonic heart beat frequency.

Model Predictions of the Embryonic Pacemaking and E-C Coupling Defects

During the early embryonic cardiac development, genetic disruption of the ion channel proteins regulating excitability (Stieber et al., 2003) or calcium influx (Weissgerber et al., 2006) as well as proteins involved in cardiomyocyte calcium handling (Takeshima et al., 1998; Wakimoto et al., 2000) lead to drastic changes in calcium signaling and heart rate, with a consequent increase in embryonic lethality. We have shown (Figs. 3, 4, 6, and 7) that our model reproduces faithfully the normal features of the Ca^{2+} signaling and excitability of E9-E11 myocytes. For further validation of our mathematical model, we tested if our model reproduces and explains the functions of the cardiomyocytes from genetically engineered mouse models previously reported to have compromised embryonic E-C coupling and/or pacemaking.

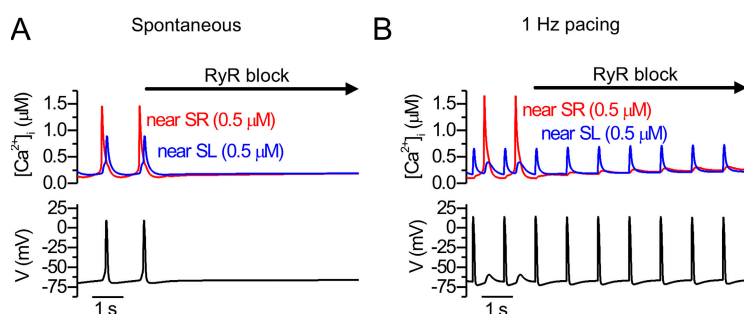


Figure 6. Simulated effect of RyR block. The near-SL and near-SR cytosolic $[\text{Ca}^{2+}]$ and APs are shown from simulations of (A) spontaneous and (B) electrically excited activity. The RyR block was applied after three control E-C coupling cycles.

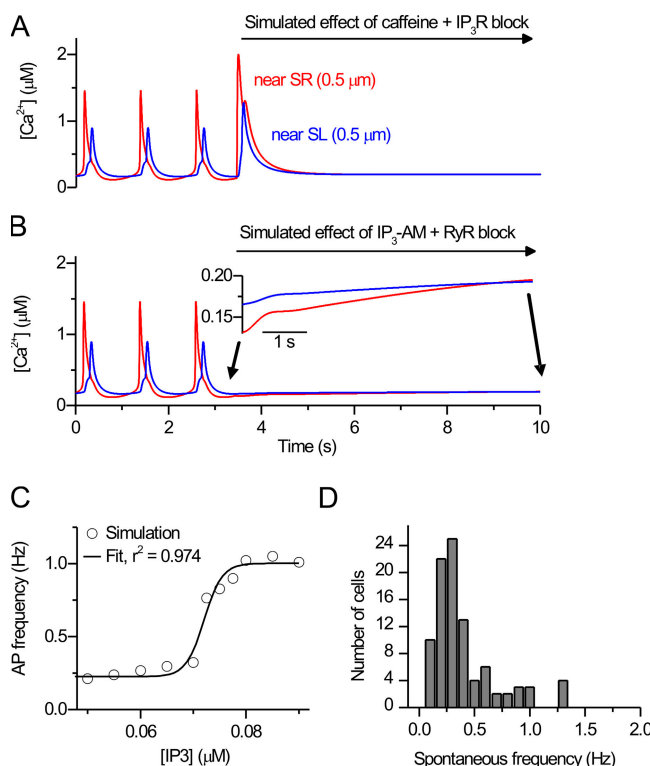


Figure 7. Simulated stimulation of RyR and IP_3 R. (A) The combined effect of caffeine (see Materials and methods) and IP_3 R block was simulated during simulation of spontaneous activity. (B) The combined effect of IP_3 -AM increasing the $[IP_3]$ slowly (see Materials and methods) and RyR block was simulated during simulation of spontaneous activity. For A and B, the near-SL and near-SR cytosolic $[Ca^{2+}]$ are shown. (C) The steady-state spontaneous AP frequency versus $[IP_3]$ (circles) with a sigmoidal fit to the data (solid line). When increasing $[IP_3]$ to values of 0.08 μM and above, arrhythmias were observed increasingly. (D) The experimentally recorded distribution of the frequencies of the spontaneous activity in E9-E11 mouse cardiomyocytes ($n = 94$). The raw data are from Rapila et al. (2008).

The hyperpolarization-activated cardiac “pacemaker” current I_f is encoded by three genes, HCN1, HCN2, and HCN4 (Yasui et al., 2001). It has been suggested that I_f is responsible for generating the spontaneous activity in embryonic ventricular cardiomyocytes (Yasui et al., 2001) as well as in specialized pacemaker cells (Stieber et al., 2003). Genetic ablation of the HCN4 reduces I_f in E10.5 mouse cardiomyocytes by $\sim 75\%$, with concomitant slowing of the heart rate by $\sim 35\%$, leading to embryonic lethality without structural anomalies between E9.5 to 11.5 (Stieber et al., 2003). In the model, reduction of the I_f from its the normal, measured density slows down the frequency of the spontaneous Ca^{2+} signals and APs, in line with the results from HCN4 $^{-/-}$ cardiomyocytes (Stieber et al., 2003) (Fig. 8, A and B). On the other hand, up to twice an increase of I_f has very little effect on the spontaneous rate of the individual myocyte, although it suppresses the amplitude of the APs (Fig. 8, A and B). Our experiments (Fig. 2 B) (Rapila et al., 2008)

and modeling (Figs. 6 and 8 A) indicate that neither I_f current density nor the voltage activation range (~ -70 mV threshold) of embryonic I_f is sufficient for initiating spontaneous V_m oscillations and APs at the resting potential (-57.2 ± 0.9 mV) (Rapila et al., 2008) of E9-E11 myocytes. However, the current density affects the excitability of the membrane by two additional mechanisms (Fig. 8, B and C), which might contribute to the phenotype of HCN4 $^{-/-}$ mice hearts. First, I_f current is partly carried by Na^+ ions; therefore, the I_f current density will effect the cytosolic $[Na^+]_i$ and consequently modulate the NCX current, which will be augmented at lower I_f densities (lower $[Na^+]_i$) and suppressed at higher I_f densities (higher $[Na^+]_i$) (Fig. 8 B). Second, because I_f is one of the depolarizing currents in embryonic myocytes, reduction of the current density will affect the excitability and the resting potential of the membrane (Fig. 8 C). Even though our experiments and modeling do not suggest a central role for I_f in developing E9-E11 ventricular myocytes, these results do not rule out the possibility that when the true pacemaker cells develop, the I_f current would have a central role in regulating the embryonic heartbeat. Interestingly, it has been suggested that also in fully developed pacemaker cells this SR-originated activity could contribute to the spontaneous activity (Bogdanov et al., 2001).

According to our experiments (Rapila et al., 2008), the NCX has a crucial role in embryonic cardiomyocytes in linking the spontaneous calcium activity with the membrane voltage. Therefore, it is not a surprise that ablation of the cardiac NCX isoform NCX1 results in embryonic lethality before E10, severe cardiomyocyte malformations, and lack of spontaneous heartbeats (Wakimoto et al., 2000). In line with the function of E9.5 NCX1 $^{-/-}$ in mouse cardiac myocytes, our model predicts that lack of NCX activity prevents triggering of the AP and decreases the spontaneous activity due to cytosolic calcium accumulation, incapacitating the calcium release. Although mouse embryos with targeted inactivation of NCX1 lack spontaneous heartbeats, cardiomyocytes isolated from NCX1-null embryos are still excitable and generate Ca^{2+} signals when electrically stimulated (Koushik et al., 2001). In line with this, model cells with reduced NCX current density generate cytosolic Ca^{2+} transients when stimulated, but during pacing calcium accumulates in the cytosol because of the reduced calcium extrusion capacity (Fig. 9). On the other hand, overexpression of NCX also inhibits spontaneous activity by depleting the calcium stores, but additionally leads to a hyperexcitable membrane and arrhythmias during external pacing (Fig. 9).

One of the few genetic models highlighting the role of the intracellular calcium stores during cardiac development is the mouse model lacking calreticulin (Mesaeli et al., 1999), a ubiquitous SR Ca^{2+} buffer expressed in cardiac myocytes during embryonic development.

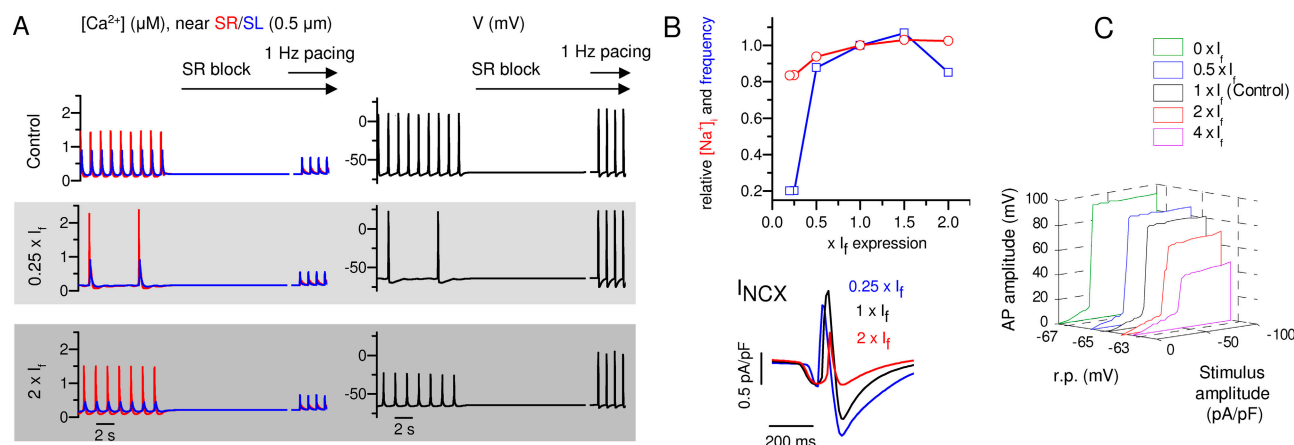


Figure 8. The simulated effect of genetic modification of the I_f . (A) Simulated effects of ablation ($0.25\times$) and overexpression ($2\times$) of I_f . The near-SL and near-SR cytosolic $[Ca^{2+}]$ and APs are shown during spontaneous activity, which is followed by an application of SR Ca^{2+} flux block and 1-Hz electrical excitation. (B) Relative changes in $[Na^+]_i$ and spontaneous beating frequency by altered I_f expression. Insert shows the I_{NCX} with different I_f expression levels ($0.25\times$, $1\times$, and $2\times$). (C) 3-D plot of the effect of varying I_f current density on the excitability and AP amplitude at different resting potentials.

Ablation of the calreticulin gene is lethal before E18 due to severe cardiac malformation and impaired function (Mesaali et al., 1999). In our model, the simulated reduction of calreticulin reduces the SR Ca^{2+} buffering and release, eventually stopping the spontaneous activity (Fig. 10 A). Overexpression of calreticulin has been reported to cause lower heart rate during embryonic development and cardiac failure and sudden cardiac death during postnatal development (Nakamura et al., 2001). In our model, the simulated overexpression results similarly in a reduced frequency of the spontaneous calcium releases with increases in released and SR Ca^{2+} (Fig. 10 A). These experimental findings (Mesaali et al., 1999; Nakamura et al., 2001) and our simulations predict that the relationship between the amount of calreticulin and the spontaneous beating rate is a bell-

shaped curve (Fig. 10 B). With both reduced and increased calreticulin content, membrane excitability and voltage-activated calcium influx are retained. However, with calreticulin overexpression, CICR is enhanced due to increased SR calcium content and release, which leads to arrhythmic spontaneous calcium releases and APs between stimulated APs.

DISCUSSION

Here, we present a mathematical model of E–C coupling and pacemaking of E9–E11 mouse ventricular cardiomyocytes. The model explains how these two separate modes for producing Ca^{2+} signals, the spontaneous activity originating from the SR triggering APs via NCX and the externally initiated AP-driven activity triggering

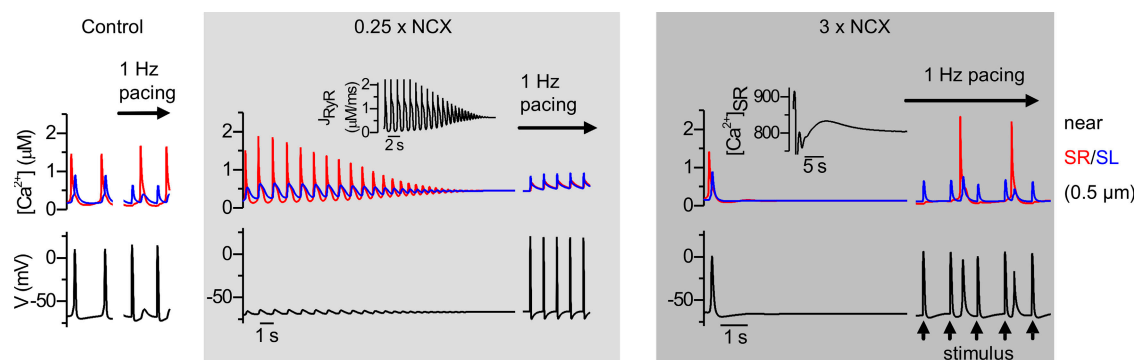


Figure 9. Effects of varying I_{NCX} density on the simulated calcium signals and membrane voltage of embryonic cardiomyocytes. Decreased I_{NCX} ($0.25\times$ control) causes cytosolic calcium accumulation and stops the spontaneous activity (middle) by altering calcium flux through RyRs (J_{RyR} , insert). Upon simulated external electrical stimulation, the model produces cytosolic calcium transients and APs, where calcium transients rely on calcium flux through voltage-activated calcium channels. Increased I_{NCX} ($3\times$ control) enhances calcium extrusion, depleting the SR calcium stores (insert), thus stopping the spontaneous activity. The model cell retains its excitability, but due to lower $[Ca^{2+}]_i$ levels facing RyRs, calcium influx can only induce sporadic SR calcium releases, thus causing irregular activity (right panels).

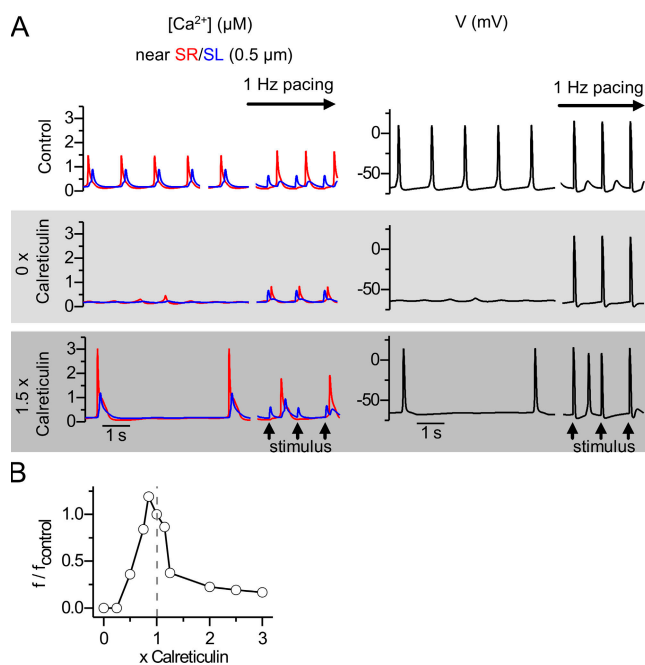


Figure 10. Effects of varying calreticulin Ca^{2+} buffer in SR on the simulated calcium signals and membrane voltage of embryonic cardiomyocytes. (A) Ablation of SR calreticulin content inhibits the spontaneous activity and reduces the stimulated calcium signals (middle row), whereas increased calreticulin content (1.5× control) lowers the frequency but increases the amplitude of both spontaneous and stimulated calcium signals. During stimulated APs, spontaneous calcium releases ensue due to overly large SR calcium content. (B) Effect of SR calreticulin content on the relative spontaneous frequency ($f/f_{control}$, Hz) of APs in the model cell.

CICR, coexist in individual cardiomyocytes. In addition to normal myocyte function, our mathematical model elucidates the E–C coupling and underlying mechanisms of the phenotypes of genetically engineered embryonic mouse models. Based on this validation, our mathematical model is the first comprehensive description of how the embryonic heartbeats are generated and regulated in E9–E11 cardiomyocytes.

Limitations of the Model

The delay from SR Ca^{2+} release to AP upstroke is larger in our model than in the experiments (Rapila et al., 2008). This is due to the approximation of the shape of the model cell to a sphere with radial symmetry. The dimensions of real cells are more similar to a flat ellipsoid. Consequently, there is variability in the diffusion distance between SL and SR and in the diffusion restriction in different parts of the cell. The local Ca^{2+} concentrations and consequently I_{NCX} are thus larger in parts of real cells, resulting in faster activation of the AP than in our model. In a more realistic ellipsoid-shaped model cell, the description of the diffusion would require three coordinates. The $[Ca^{2+}]$ would have spatial differences in directions parallel to the SL and SR surfaces, and the

function of Ca^{2+} transporting ion channels would need to be calculated separately in all points of the SL and SR surface grid. This would increase the computational cost exponentially and severely limit the practical usability of the model. Our model is capable of explaining the embryonic E–C coupling and pacemaking mechanisms and underlying mechanisms of several genetically engineered embryonic mice. The spherical shape is thus a fair compromise between computational efficiency and the validity of our model.

The Simulated Ca^{2+} Oscillations in E9–E11 Cardiomyocytes
The spontaneous Ca^{2+} oscillations between cytosol and SR/ER have been modeled previously in other cell types than cardiac myocytes (Deyoung and Keizer, 1992; Keizer and Levine, 1996; Sneyd et al., 2003). The models have included the Ca^{2+} -ATPase pump and IP_3R (Deyoung and Keizer, 1992) or RyR (Keizer and Levine, 1996) or both of these receptors (Sneyd et al., 2003), as Ca^{2+} routes between the SR/ER and cytosol. These models produce cytosolic Ca^{2+} oscillations at the rate of ~ 0.1 – 0.01 Hz (Deyoung and Keizer, 1992; Keizer and Levine, 1996; Sneyd et al., 2003), whereas the spontaneous Ca^{2+} oscillations in the E9–E11 cardiomyocytes had a frequency of ~ 0.1 – 1.3 Hz (Rapila et al., 2008). Here, we showed with modeling that this rapid oscillation (~ 1 Hz) can also be theoretically produced by the combined activity of $RyRs$, IP_3Rs , and SERCA (Fig. 3). The basis of this activity is the $[IP_3]$ -dependent IP_3R Ca^{2+} leak, which triggers the large Ca^{2+} releases via RyR (Figs. 3 and 7) and thereby increases the endogenously low spontaneous opening rate of $RyRs$ (Keizer and Levine, 1996). Thus, as in the experiments (Rapila et al., 2008), the magnitude of the IP_3R Ca^{2+} leak regulates the frequency of the Ca^{2+} oscillations and APs triggered by this oscillation.

In line with our experiments (Rapila et al., 2008), the RyR , IP_3R , and SERCA all play obligatory roles in producing oscillations (Fig. 6 and Fig. S1). However, as long as all of these components are present to some extent, the oscillation seems to be robust, as it was maintained even with $\pm 25\%$ change in the amount of RyR , IP_3R , or SERCA (unpublished data). The cardiac myocytes undergo dramatic changes during development; therefore, the SR-originated oscillation might be a stable backup that guarantees the cell's capability to maintain its activity in these varying conditions.

Electrophysiology of the E9–E11 Cardiomyocytes

Here, we presented the first complete characterization of membrane ion currents in E9–E11 mouse ventricular cardiomyocytes (Fig. 2). Based on our simulations and experiments (Rapila et al., 2008), the NCX is the most crucial ion current regulating the activity of the embryonic cardiomyocytes. In E9–E11 cardiomyocytes, the I_{NCX} triggers membrane depolarization during spontaneous activity and regulates the r.p. and intracellular

[Ca²⁺] (Table I and Figs. 3 and 4). These multiple roles of I_{NCX} explain the severe dysfunctions in the simulated E–C coupling and pacemaking with altered amounts of functional NCX (Fig. 9) and the embryonic lethality of the embryos lacking NCX1 (Wakimoto et al., 2000).

It has been suggested that I_f generates the spontaneous activity in embryonic cardiomyocytes (Stieber et al., 2003). Although we found a significant amount of I_f from E9–E11 myocytes, results in this and our accompanying paper in this issue suggest that the I_f does not initiate the spontaneous activity in E9–E11 cardiomyocytes. The pharmacological inhibition of the I_f in the experiments (Rapila et al., 2008) and the simulated overexpression and down-regulation of the I_f did not stop the rhythmic Ca²⁺ activity triggering the contraction and APs via NCX. The I_f in E9–E11 cardiomyocytes shows a significant active current only at membrane voltages lower than r.p. (Fig. 2 B); thus, even a doubled amount of current in E9–E11 myocytes cannot generate spontaneous APs (Fig. 8 A). Similarly to I_f, we found a small amount of functional T-type Ca²⁺ channel current in E9–E11 cardiomyocytes (Fig. 2). The specific method to measure T-type current would have been recording it as an Ni²⁺-sensitive current (Furukawa et al., 1992). However, the T-type current was separated sufficiently from the L-type current based on voltage clamps from different holding potentials as described previously (Niwa et al., 2004).

According to model simulations, the modes for spontaneous Ca²⁺ oscillations and AP-induced Ca²⁺ transients can be separated on the basis of their resting potential boundaries (Fig. 5). We found that spontaneous calcium release can operate effectively at relatively depolarized membrane potentials, whereas AP-induced CICR is favored when the membrane potential is more hyperpolarized. This difference between the excitation modes in respect to their r.p. boundaries may represent the order of recruitment of these modes during development because the cardiomyocyte resting potential hyperpolarizes during the progress of fetal development (Reppel et al., 2007). During cell migration in early development the cells are isolated from others (Buckingham et al., 2005), and even with depolarized r.p., their spontaneous activity guarantees that their activity is maintained. Later during development, the cells with more negative r.p. values form a stable tissue wherein the phenotype is shaped toward that of non-spontaneously active adult ventricular cardiomyocytes, which form coordinated contraction induced by an external stimulus (Kamino, 1991). Also, it is energetically cheaper not to provide the AP-driven mode until it is required for efficient and more coordinated contraction because based on our simulations, maintaining a hyperpolarized r.p. requires larger NaK-ATPase activity and therefore induces a higher ATP consumption rate (unpublished data).

Regulation of the Embryonic E–C Coupling and Heartbeat

The physical structure of E9–E11 cells sets boundary conditions for the E–C coupling and pacemaking. The lack of T tubules in E9–E11 myocytes results in loose coupling between SR and SL ion channels and other components. This limits the possible heartbeat frequency because a certain time is required for Ca²⁺ diffusion between SR and SL. Furthermore, any alterations in the shape and the size of the cytosol affect the dynamics of the cytosolic Ca²⁺ signals, further modulating the heartbeat frequency. Due to the lack of T tubules and loose spatial coupling between I_{CaL} and RyR, a relatively large SL Ca²⁺ intrusion is required for a strong enough Ca²⁺ signal to diffuse through the cytosol and initiate CICR from SR. In the adult mouse ventricular myocyte, with tight I_{CaL} and RyR coupling, only ~10% of total cytosolic Ca²⁺ intrusion originates from SL and ~90% from SR during CICR (Maier et al., 2003). Our simulations suggest that during AP-induced CICR, ~42% of cytosolic Ca²⁺ intrusion occurs from the SL and ~58% from the SR (Fig. 4 C). In addition, our results suggest that a strong SR function is essential for spontaneous activity in embryonic cardiomyocytes as well as for synchronizing the contractile activity via the AP-driven mode.

On the basis of our results, several contributing mechanisms for the regulation of the beating rate of the embryonic hearts can be suggested. In general, because the spontaneous activity originates solely from the single cell and it is not controlled by any outside triggering mechanism, several parameters within the cell may affect the rate of activity. A dynamic regulation in the time scale of seconds could be addressed via regulation of the activity of IP₃Rs, RyRs, and SERCA. One example of the direct modulation would be the [IP₃], which was shown here to strongly regulate the cardiomyocyte beating frequency (Fig. 7). The upper boundary of the [IP₃]-dependent beating frequency is limited because the increment of [IP₃] also depletes the SR Ca²⁺ required for spontaneous releases. Subsequently, the relationship between cardiomyocyte beating frequency and [IP₃] is a bell-shaped curve. The activity of SERCA could modulate heart rate because altering the refilling velocity of the SR alters the kinetics of the relaxation phase of the Ca²⁺ oscillation as well as Ca²⁺ leak through IP₃Rs. Based on this, it is possible in theory that the dynamic regulatory mechanisms directly or indirectly affecting SERCA function, such as the β-adrenergic pathway, will regulate heart rate by modulating the SR Ca²⁺ uptake. In a slower time scale, the heartbeat could be obviously regulated by altering the expression levels of RyR, IP₃R, and SERCA as well as calreticulin (Fig. 10 B). The SL ion channels also affect the heart rate. They may contribute directly, such as I_{CaL} and I_{NCX}, or indirectly, such as the I_f (Fig. 8), to the kinetics of Ca²⁺ fluxes at the SL and furthermore to the SR Ca²⁺ content and dynamics.

Here, we have presented a characterization and a mathematical model of E–C coupling and pacemaking in early embryonic (E9–E11) mouse ventricular cardiomyocytes. To develop the model, we presented novel approaches in cardiomyocyte modeling. The model includes an implementation of a noncommon pool cytosol and oscillatory SR dynamics incorporated with SL ion current dynamics as characterized in our experiments. The model explains the underlying mechanisms behind the functional dualism of these cells (Rapila et al., 2008). The model reproduces the SR-driven spontaneous activity and the AP-driven externally evoked activity. The model also elucidates the mechanisms behind the altered E–C coupling and pacemaking in genetically modified embryos. The current understanding of the embryonic cardiomyocyte E–C coupling and pacemaking is shaped by the suggestions of the underlying mechanisms based on experimental results, which so far have been controversial. This study shows by mathematical modeling how several of the suggested mechanisms can operate in parallel to control the initiation and regulation of the embryonic heartbeat.

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