

Muscle Chloride Channel Dysfunction in Two Mouse Models of Myotonic Dystrophy

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Muscle degeneration and myotonia are clinical hallmarks of myotonic dystrophy type 1 (DM1), a multisystemic disorder caused by a CTG repeat expansion in the 3' untranslated region of the myotonic dystrophy protein kinase (*DMPK*) gene. Transgenic mice engineered to express mRNA with expanded (CUG)₂₅₀ repeats (*HSA*^{LR} mice) exhibit prominent myotonia and altered splicing of muscle chloride channel gene (*Clcn1*) transcripts. We used whole-cell patch clamp recordings and nonstationary noise analysis to compare and biophysically characterize the magnitude, kinetics, voltage dependence, and single channel properties of the skeletal muscle chloride channel (ClC-1) in individual flexor digitorum brevis (FDB) muscle fibers isolated from 1–3-wk-old wild-type and *HSA*^{LR} mice. The results indicate that peak ClC-1 current density at –140 mV is reduced >70% (–48.5 ± 3.6 and –14.0 ± 1.6 pA/pF, respectively) and the kinetics of channel deactivation increased in FDB fibers obtained from 18–20-d-old *HSA*^{LR} mice. Nonstationary noise analysis revealed that the reduction in ClC-1 current density in *HSA*^{LR} FDB fibers results from a large reduction in ClC-1 channel density (170 ± 21 and 58 ± 11 channels/pF in control and *HSA*^{LR} fibers, respectively) and a modest decrease in maximal channel open probability (0.91 ± 0.01 and 0.75 ± 0.03, respectively). Qualitatively similar results were observed for ClC-1 channel activity in knockout mice for muscleblind-like 1 (*Mbnl1*^{ΔE3/ΔE3}), a second murine model of DM1 that exhibits prominent myotonia and altered *Clcn1* splicing (Kanadia et al., 2003). These results support a molecular mechanism for myotonia in DM1 in which a reduction in both the number of functional sarcolemmal ClC-1 and maximal channel open probability, as well as an acceleration in the kinetics of channel deactivation, results from CUG repeat-containing mRNA molecules sequestering Mbnl1 proteins required for proper *CLCN1* pre-mRNA splicing and chloride channel function.

INTRODUCTION

Myotonic dystrophy type 1 (DM1) is the most common adult-onset form of muscular dystrophy with an estimated frequency of 1 in 7,400 (Harper, 1989). DM1 is characterized by dominantly inherited ocular cataracts, cardiac conduction defects, hypogonadism, muscle weakness, and an increase in skeletal muscle excitability resulting in prominent myotonia. Interestingly, DM1 is not caused by mutations in the genes that encode either the skeletal muscle sodium (*SCN4A*) or chloride (*CLCN1*) channel. Rather, DM1 is linked to a trinucleotide (CTG) repeat expansion in the 3' untranslated region of the myotonic dystrophy protein kinase gene (*DMPK*) (Brook et al., 1992). The trinucleotide repeat expansion leads to the production of *DMPK* transcripts that are not exported from the nucleus (Taneja et al., 1995; Davis et al., 1997), and thus result in a decrease in *DMPK* translation and expression (Furling et al., 2001). Mounsey et al. (2000) found that sodium channels in skeletal muscle fibers obtained from both *Dmpk*^{+/-}

and *Dmpk*^{-/-} mice exhibit incomplete inactivation, late channel reopenings, and a persistent sodium current. These results suggest that altered sodium channel inactivation contributes to increased muscle excitability and susceptibility to myotonia in DM1 (Mounsey et al., 2000). However, *Dmpk*-dependent changes in skeletal muscle sodium channel inactivation are apparently not sufficient for increased susceptibility to myotonia since *Dmpk*^{-/-} mice are not myotonic. Moreover, a second form of DM (DM2) results from a similar repeat expansion (CCTG) in intron 1 of a completely different gene (zinc finger protein-9 or *ZNF9* gene) (Liquori et al., 2001). Changes in the activity of a small conductance, calcium-activated potassium channel have also been suggested to contribute to the increased incidence of myotonia in DM (Behrens et al., 1994; Kimura et al., 2003).

Abbreviations used in this paper: 9AC, 9-anthracene carboxylic acid; ClC-1, chloride channel type 1; DMPK, myotonic dystrophy protein kinase; DM1, myotonic dystrophy type 1; FDB, flexor digitorum brevis; *HSA*^{LR}, human skeletal actin long repeat mouse; MBNL1, muscleblind-like 1; SCN4A, skeletal muscle voltage-dependent sodium channel.

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An attractive alternative hypothesis for DM pathogenesis in humans involves an RNA transdominant mechanism in which CUG repeat-containing mRNA transcripts from the mutant *DMPK* allele accumulate in the nucleus and sequester critical regulators of RNA processing for a specific subset of genes (e.g., *CLCN1*) (Mankodi et al., 2002). To determine the effects of CUG repeat expansion on skeletal muscle, Mankodi et al. (2000) developed a transgenic mouse model of DM1 (*HSA^{LR}*) that exhibits high level muscle-specific expression of mRNA for human skeletal actin (HSA) harboring ~250 CUG repeats in the 3' untranslated region of the gene. *HSA^{LR}* mice exhibit prominent myotonia and aberrant splicing of *Cln1* pre-mRNA, including a high incidence of inclusion of a novel exon (exon 7a) that results in a frame shift and premature termination in the CIC-1 protein. Additionally, 76% of *Cln1* from *HSA^{LR}* mice was aberrantly spliced with 69% resulting in various premature terminations. Similar transdominant alterations in *CLCN1* mRNA splicing were also observed in muscle obtained from human DM1 and DM2 patients (Mankodi et al., 2002). Although the truncated CIC-1 products do not form functional heterodimeric chloride channels, coexpression with wild-type CIC-1 results in dominant-negative effects on chloride channel activity (i.e., reduced current density and accelerated channel deactivation) (Berg et al., 2004).

Muscleblind-like 1 (MBNL1) proteins are regulators of mRNA splicing (Ho et al., 2004) that bind with high affinity to expanded CUG or CCUG repeat RNA. MBNL1 proteins are sequestered into nuclear RNA foci in skeletal muscle of *HSA^{LR}* mice (CUG), as well as DM1 (CUG) and DM2 (CCUG) patients (Mankodi et al., 2001). In support of a pathogenic role for loss of MBNL1 function in DM pathogenesis, skeletal muscle of *Mbn1* knockout mice (*Mbn1^{ΔE3/ΔE3}*) also exhibits prominent myotonia, aberrant *Cln1* mRNA splicing, and reduced CIC-1 protein expression (Kanadia et al., 2003). While evidence supports an overall reduction in total membrane chloride conductance (G_{Cl}) in skeletal muscle of *HSA^{LR}* mice (Mankodi et al., 2000), the effects of CUG repeat expansion and *Mbn1* deficiency in mice on the functional expression, kinetics, voltage dependence, and single channel properties of muscle CIC-1 channels have not been determined.

The aim of this study was twofold. First, we set out to characterize the functional expression and biophysical properties (kinetics, voltage dependence, single channel properties) of CIC-1 channels in single skeletal muscle fibers in whole-cell patch clamp experiments. Chloride channel conductance in skeletal muscle has been reported previously using double sucrose (Duval and Leoty, 1980), vaseline gap (Fahlke and Rudel, 1995), and two-electrode (Chen and Jockusch, 1999) voltage clamp techniques (for review see Bretag, 1987). However, no studies have characterized macroscopic

(or unitary) CIC-1 properties in whole-cell patch clamp experiments of native skeletal muscle preparations. This is presumably because CIC-1 current density is thought to be too high and adult muscle fibers too large to provide an adequate voltage clamp in most preparations. Here we circumvented this problem by using very low resistance pipettes (~0.5 MΩ) to patch clamp relatively small, freshly dissociated flexor digitorum brevis (FDB) muscle fibers from young (10–21 d old) mice. This approach enabled biophysical characterization of CIC-1 channel activity in native mammalian skeletal muscle fibers. In addition, we provide a comprehensive comparison of endogenous CIC-1 biophysical properties with that observed following heterologous (in HEK293 cells) and homologous (in skeletal myotubes) expression of the cloned murine CIC-1 channel (mCIC-1). A second aim of this study was to compare the expression and biophysical properties of CIC-1 channel activity in FDB fibers obtained from WT mice with those observed in two different mouse models of human myotonic dystrophy (*HSA^{LR}* and *Mbn1^{ΔE3/ΔE3}* mice).

MATERIALS AND METHODS

Construction and Expression of mCIC-1 in HEK293 Cells and Skeletal Myotubes

A cDNA encoding the murine skeletal muscle chloride channel (mCIC-1; NM_013491) was generated using reverse transcription of mRNA isolated from skeletal muscle of WT mice as previously described (Mankodi et al., 2002). Murine CIC-1 exhibits 87% and 96% amino acid identity with human and rat CIC-1, respectively. The cDNA was ligated into the NheI/XhoI sites of pShuttle-IRES-hrGFP-1 (Stratagene). HEK293 cells (Stratagene) were transfected at 50% confluence using Lipofectamine 2000 (Invitrogen) according to manufacturer recommendations. Primary cultures of myotubes were prepared from myoblasts obtained from skeletal muscle of newborn type 1 ryanodine receptor null (dyspedic) mice as previously described (Nakai et al., 1996). Dyspedic myotubes were used as a homologous mCIC-1 expression system because they lack endogenous chloride currents (see Fig. 2 B, upright triangles) and remain quiescent during nuclear cDNA microinjection. Expression of mCIC-1 in dyspedic myotubes was achieved by nuclear microinjection of 0.02 μg/μl mCIC-1-IRES-hrGFP-1 6–8 d after the initial plating of myoblasts. Expressing HEK293 cells and skeletal myotubes were identified 24–72 h after transfection or nuclear microinjection, respectively, by monitoring for GFP fluorescence. GFP-positive cells/myotubes were then used in whole-cell patch clamp experiments as described below.

Preparation of FDB Muscle Fibers

Skeletal muscle fibers were isolated from FDB muscle obtained from 10–20-d-old WT, *HSA^{LR}*, and *Mbn1^{ΔE3/ΔE3}* mice, as previously described (Beam and Knudson, 1988). All animals were housed in a pathogen-free area at the University of Rochester School of Medicine and Dentistry (URSMD). Animals were anesthetized and killed by procedures that were reviewed and approved by the University Committee on Animal Resources at URSMD. In brief, FDB muscles were dissected and mechanically cleaned of connective tissue in a Ringer solution containing (in mM): 146 NaCl, 5 KCl, 2 CaCl₂, 1 MgCl₂, 10 HEPES, pH 7.4 with NaOH (Beam and Knudson, 1988). Muscles were then shaken for 40 min at 37°C in

TABLE I
Parameters of Linear Properties and Relative Open Probabilities

	Linear properties				$P_{o,rel}$	
	n	C_m pF	R_s $k\Omega$	τ_m μs	$V_{1/2}$ mV	k mV
mClC-1 HEK cells	12	13 ± 1	495 ± 32	176 ± 5	-61.5 ± 4.2	25.0 ± 0.7
mClC-1 myotubes	4	184 ± 41	1,039 ± 93	219 ± 9	-74.8 ± 1.7	25.1 ± 3.1
WT FDB fibers (18–20 d)	8	620 ± 68	391 ± 77	487 ± 63	-66.0 ± 5.6	29.0 ± 3.2
HSA ^{L-R} FDB fibers (18–20 d)	15	704 ± 25	393 ± 47	488 ± 27	-60.8 ± 4.4	27.7 ± 2.9
<i>Mbnl1</i> ^{+/+} FDB fibers (9–14 d)	22	512 ± 37	811 ± 50	377 ± 25	-72.3 ± 2.6	27.0 ± 0.9
<i>Mbnl1</i> ^{ΔE3/ΔE3} FDB fibers (9–14 d)	16	511 ± 41	787 ± 60	358 ± 60	-75.8 ± 2.1	23.4 ± 1.1

1 mg/ml collagenase A (Roche) dissolved in Ringer's solution. Individual FDB fibers were then dissociated by trituration using Pasteur pipettes of decreasing bore size. Only fibers exhibiting clear striations and clean surfaces were chosen for electrophysiological recordings. All experiments were conducted at room temperature on fibers obtained within 8 h of isolation.

Macroscopic Recordings of ClC-1 Currents

ClC-1 currents were measured using the whole-cell variant of the patch clamp technique (Hamill et al., 1981) and recorded in an external solution consisting of (in mM) 145 TEA-Cl, 10 CaCl₂, 10 HEPES, and 3 μM nifedipine (pH 7.4). Low resistance patch pipettes (0.5 MΩ for FDB fibers/myotubes and 1–2 MΩ for HEK293 cells) were filled with an internal recording solution consisting of (in mM) 110 Cs-aspartate, 30 CsCl, 5 MgCl₂, 10 Cs₂-EGTA, and 10 HEPES (pH 7.4). These conditions provide adequate block of sodium (0 Na), calcium (nifedipine), and potassium (0 K/TEA/Cs) currents. In the cell-attached configuration, seal resistances of ≥5 GΩ were achieved in all experiments. After establishment of the whole-cell configuration in FDB fibers and expressing myotubes, a dialysis period of 8–10 min was used to ensure complete exchange with the internal solution. Ionic currents were compensated for series resistance (>90%), filtered at 2 kHz using an Axopatch 200A amplifier (Molecular Devices), digitized at 10 kHz using a 16-bit converter (Digidata 1322A; Axon Instruments), and acquired/analyzed using the pCLAMP 9 software suite (Molecular Devices).

Chloride currents were elicited using a voltage protocol (see Fig. 1, top) similar to that used widely by other investigators studying ClC-1 channels expressed in heterologous systems. From a holding potential of -40 mV (near the calculated chloride equilibrium potential of -35.8 mV), an initial 200-ms depolarization to +60 mV was used to fully activate ClC-1 channels, followed by a second 250-ms (350 ms for *Mbnl1*^{ΔE3/ΔE3} fibers) voltage step of variable amplitude (between -140 mV and +60 mV in 10-mV increments), and then a final 200-ms voltage step to -100 mV (-110 mV for *Mbnl1*^{ΔE3/ΔE3} fibers). This voltage protocol was first delivered in the absence and then following the addition of 1 mM 9-anthracene carboxylic acid (9AC), a blocker of ClC-1 channels. Only experiments with an input resistance of ≥100 MΩ after the addition of 9AC were included in this study. Offline subtraction of currents recorded in the presence of 9AC from those recorded in its absence (9AC-sensitive currents) was used to eliminate residual leak and capacitive currents. Thus, 9AC-sensitive currents were used to define ClC-1 channel activity in this study. After block of ClC-1 currents, total cell capacitance (C_m), uncompensated series resistance (R_s), and the time constant for membrane charging (τ_m) were determined by integration of the capacity transient resulting from the average of five 10-mV depolarizing pulses applied from a holding potential of -80 mV (Table I). Current density (pA/pF) was then calculated for each record in

order to compare data across cells of different sizes. This approach enabled quantification of several fundamental features of ClC-1 activity, including (a) peak current density, (b) reversal potential, (c) kinetics of channel deactivation (i.e., two exponential fitting of current decay during the variable voltage step), and (d) the voltage dependence of relative channel open probability (from peak currents during the final voltage step). Instantaneous ClC-1 current density was plotted versus membrane voltage (V_m) and fitted according to

$$I(V) = (I_{\max} - I_0) / (1 + \exp((V_m - V_{1/2})/k)) + I_0, \quad (1)$$

where I_{\max} is the maximum current at the test potential (V_m), I_0 is a constant offset, $V_{1/2}$ is the half-maximal activation voltage, and k is a slope factor. ClC-1 currents during the variable voltage step used to quantify the kinetics of current deactivation were fitted according to the following two-exponential function:

$$I(t) = A_1[\exp(-t/\tau_1)] + A_2[\exp(-t/\tau_2)] + C, \quad (2)$$

where $I(t)$ represents current amplitude at any time t during the pulse, A_1 and A_2 represent the steady-state current amplitudes of each component with their respective time constants (τ_1 and τ_2), and C represents a time-independent current amplitude. For each test potential, the relative contribution of each current amplitude (A_1 , A_2 , and C) was calculated by dividing the absolute value by the sum of all three components (e.g., $A_1/A_{\text{total}} = A_1/[A_1 + A_2 + C]$). To determine the effect of current magnitude on channel deactivation, we analyzed the deactivation kinetics at -100 mV after 200-ms prepulses to potentials ranging from +60 mV to -80 mV (in 10-mV increments) in 18–20-d-old WT FDB fibers. The current magnitude decreased as the prepulse became more negative due to a decrease in steady-state channel open probability during the prepulse. The dependence of the kinetics of channel deactivation across different current magnitudes within the same cell was then quantified using Eq. 2, as described above.

The voltage dependence of relative channel open probability ($P_{o,rel}$) was calculated from the normalized tail current amplitude elicited in the final voltage step (at -100 mV) and fitted according to

$$P_{o,rel}(V) = P_{\min} + ((1 - P_{\min}) / (1 + \exp(-(V_m - V_{1/2})/k))), \quad (3)$$

where P_{\min} is an offset, V_m is the membrane potential, $V_{1/2}$ is the potential at which $P_o(V) = (P_{o,\max} - P_{\min})/2$, and k is a slope factor.

Nonstationary Noise Analysis

Determination of ClC-1 single channel current (i), maximal channel open probability ($P_{o,\max}$), and the number of functional ClC-1 channels (N) was calculated using nonstationary noise

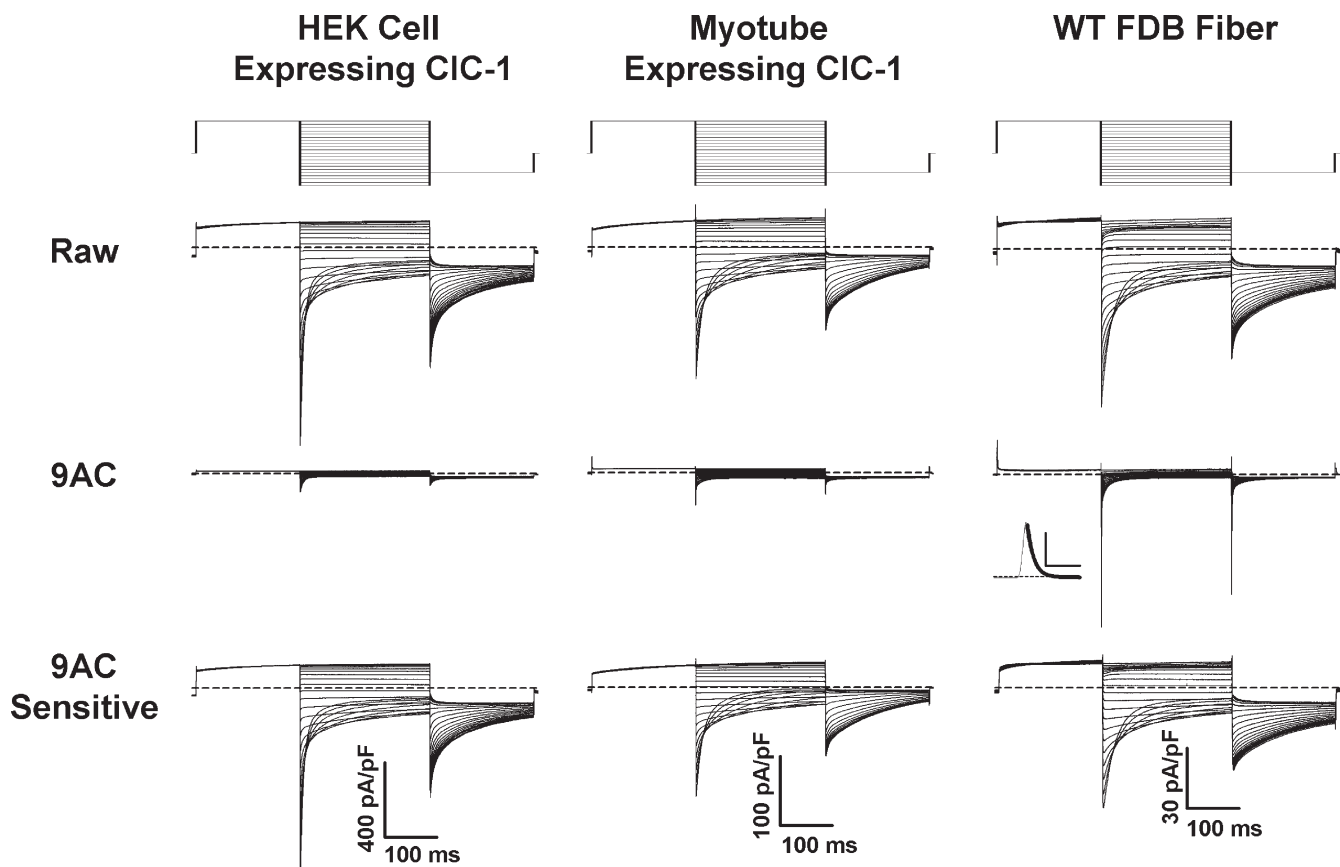


Figure 1. Chloride channel currents from mCIC-1-expressing HEK293 cells, mCIC-1-expressing mouse skeletal myotubes, and native FDB fibers obtained from 18–20-d-old WT mice. Representative whole-cell currents recorded first in the absence (Raw) and then in the presence of 1 mM 9AC (9AC) using an identical voltage protocol (top). CIC-1 currents were then quantified after offline subtraction of 9AC-insensitive currents from raw currents (9AC sensitive). (Inset) Capacitative current recorded from the WT FDB fiber resulting from the average of five 10-mV depolarizations delivered from a -80 -mV holding potential. The time constant of the capacitative current relaxation was fitted (thick line) to a first-order exponential function ($\tau_m = 339 \mu\text{s}$). Cell capacitance and access resistance deduced from the fit were 671 pF and 509 k Ω , respectively. The scale bars for the inset are 6 nA (vertical) and 2 ms (horizontal). The dashed lines represent the zero current level.

analysis (Sigworth, 1980). Mean current (I) and variance (σ^2) were calculated from 70–120 current traces (delivered at 0.2 Hz) during channel deactivation resulting from a 200-ms test pulse to -140 mV after a 100-ms prepulse to $+60$ mV. Baseline variance was measured from a 200-ms pulse to the channel reversal potential (-32 mV) delivered immediately after the test pulse. Mean background and capacitative currents calculated by averaging >20 test pulses recorded in the presence of 1 mM 9AC were used for offline subtraction. Variance was obtained by averaging the squared difference of consecutive 9AC-subtracted traces (Heinemann and Conti, 1992). To eliminate variance due to linear capacitative currents, variance measurements were initiated after $>94\%$ of the capacitance transient had decayed. The mean current (I)–variance (σ) relationships were fitted to the following parabolic equation:

$$\sigma^2 = iI - (I^2/N). \quad (4)$$

The number of ion channels (N) and the unitary current (i) were used to calculate maximal channel open probability from the peak current (I_{max}) according to

$$P_{0_{\text{max}}} = I_{\text{max}} / (iN). \quad (5)$$

Conductance values were calculated from i assuming a linear current–voltage curve at negative membrane potentials (Pusch et al., 1994). Data were analyzed using the Ana (written and provided by M. Pusch, Institute of Biophysics, Genova, Italy, http://www.ge.cnr.it/ICB/conti_moran_pusch/programs-pusch/software-mik.htm), Excel, pCLAMP, and Sigmaplot 8.0 software packages. All results are given as means \pm SEM with statistical significance ($P < 0.05$) determined using a two-tailed, unpaired Student's t test.

RESULTS

Comparison of Macroscopic CIC-1 Current Properties in Wild-Type FDB Fibers with mCIC-1-expressing HEK293 Cells and Skeletal Myotubes

A major goal of this study was to quantify the biophysical properties of CIC-1 channel activity in native skeletal muscle fibers using the whole-cell patch clamp technique. To minimize problems related to voltage clamp of large CIC-1 currents, we used low resistance (~ 0.5 M Ω) patch pipettes to voltage clamp FDB fibers from

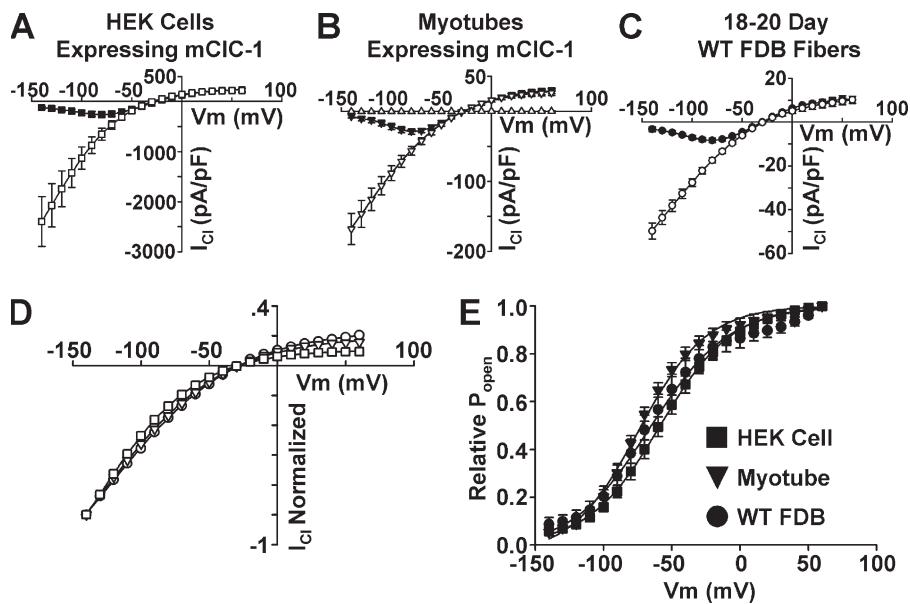


Figure 2. Macroscopic properties of expressed and native ClC-1 currents. Voltage dependence of average instantaneous (open symbols) and steady-state (closed symbols) ClC-1 currents recorded from mClC-1-expressing HEK293 cells (A; $n = 12$), mClC-1-expressing skeletal myotubes (B; $n = 4$), and native FDB fibers obtained from 18–20-d-old WT mice (C; $n = 8$). Instantaneous currents measured in control noninjected myotubes did not display appreciable ClC-1 currents (upright triangles). (D) Superimposed and normalized instantaneous current–voltage relationships obtained from mClC-1-expressing HEK293 cells (squares), myotubes (inverted triangles), and native WT FDB fibers (circles). (E) Average relative P_o - V curves for mClC-1-expressing HEK293 cells (squares), myotubes (inverted triangles), and native WT FDB fibers (circles) obtained from tail currents elicited at -100 mV. Smooth curves through each P_o - V dataset were generated using a modified Boltzmann equation (Eq. 3).

young (10–21 d old) wild-type mice. This preparation has been used previously to monitor the function and biophysical properties of native L-type Ca^{2+} channels (Beam and Knudson, 1988; Wang et al., 1999). The voltage dependence and kinetics of ClC-1 channel activation and deactivation was assessed using a voltage protocol (Fig. 1, top; see also Materials and methods) that fully activates ClC-1 channels with a strong depolarization, followed by a second voltage step of variable amplitude, and then a final voltage step to -100 mV. This protocol was delivered in the absence and then presence of 9AC (1 mM). 9AC-sensitive currents were used throughout this study as an indication of ClC-1 channel activity. Using this approach, the voltage dependence and kinetics of macroscopic 9AC-sensitive ClC-1 currents were similar in wild-type FDB fibers and in mClC-1-expressing HEK293 cells or skeletal myotubes (Figs. 1–3). Fig. 1 shows representative macroscopic ClC-1 currents recorded from an mClC-1-expressing HEK293 cell (left), an mClC-1-expressing skeletal myotube (middle), and a native FDB fiber obtained from a 19-d-old wild-type mouse (right). Currents are shown under control conditions (top), in the presence of 1 mM 9AC (middle), and following subtraction of 9AC-insensitive currents (bottom). Peak currents at -140 mV in control FDB fibers were reduced $\sim 98\%$ by 1 mM 9AC. Current density for all experiments was calculated by dividing currents by the cell capacitance determined from the average of five 10-mV depolarizing pulses from a -80 mV holding potential (inset to 9AC data in Fig. 1, right). The average cell capacitance of HEK293 cells, myotubes, and

18–20-d-old wild-type FDB fibers was 13 ± 1 pF ($n = 12$), 184 ± 41 pF ($n = 4$), and 620 ± 68 pF ($n = 8$), respectively (Table I).

The voltage dependence of the average instantaneous (open symbols) and steady-state (closed symbols) components of 9AC-sensitive currents were similar in mClC-1-expressing HEK293 cells (Fig. 2 A), mClC-1-expressing myotubes (Fig. 2 B), and native wild-type FDB fibers (Fig. 2 C). This similarity is emphasized upon superimposing normalized instantaneous current–voltage relationships (Fig. 2 D). Similarly, the voltage dependence of ClC-1 relative channel open probability ($P_{o,rel}$) assessed during the final voltage step was comparable in wild-type FDB fibers (circles), mClC-1-expressing HEK293 cells (squares), and skeletal myotubes (inverted triangles). $P_{o,rel}$ - V relationships were well described by a modified Boltzmann function (Eq. 3) with similar values for $V_{1/2}$ and k for FDB fibers ($n = 8$), HEK293 cells ($n = 12$), and myotubes ($n = 4$) (Table I). Similar values for the voltage dependence of $P_{o,rel}$ have also been reported by others after heterologous expression of human ClC-1 (Pusch et al., 1995).

Initial inspection of the 9AC-sensitive currents shown in Fig. 1 suggested that the rate of ClC-1 deactivation was somewhat faster after expression of mClC-1 in HEK293 cells compared with that observed in either mClC-1-expressing myotubes or native FDB fibers. Therefore, as a fourth measure of ClC-1 function (in addition to instantaneous, steady-state, and $P_{o,rel}$ -voltage relationships), we also compared the voltage dependence of the kinetics of ClC-1 channel deactivation

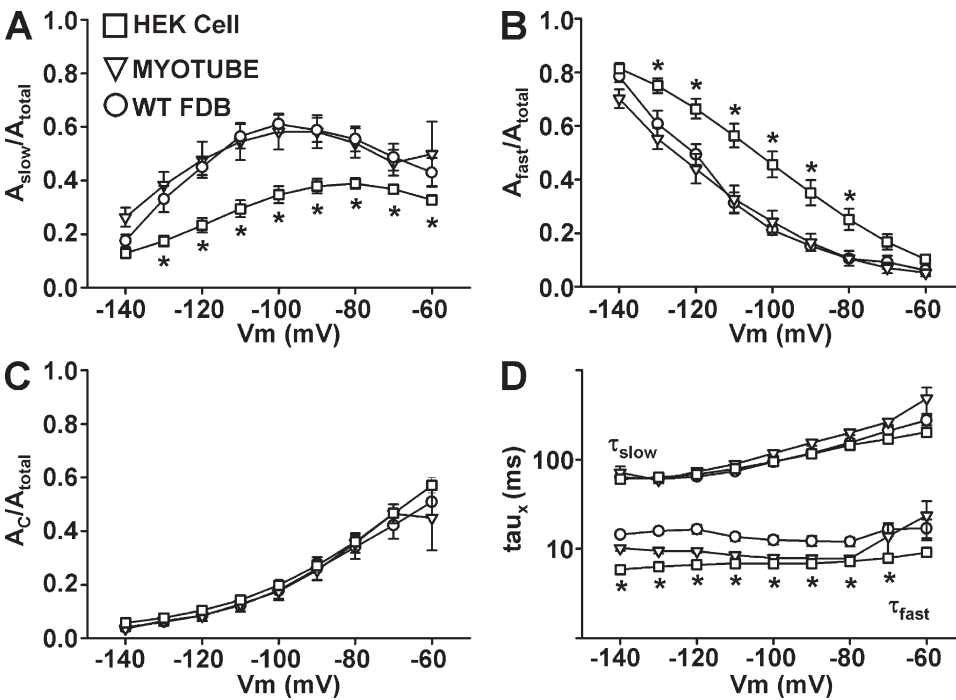


Figure 3. Deactivation kinetics of expressed and native ClC-1 channels. Voltage dependence for the relative contributions of the slow (A), fast (B), and nondeactivating (C) gating components of ClC-1 deactivation in mClC-1-expressing HEK293 cells (squares; $n = 12$), mClC-1-expressing myotubes (triangles; $n = 4$), and native FDB fibers obtained from 18–20-d-old WT mice (circles; $n = 8$). (D) Voltage dependence of the time constants for the fast (lower symbols) and slow (upper symbols) components of ClC-1 deactivation. *, $P \leq 0.05$ HEK293 cells compared with WT FDB fibers.

in native FDB fibers and after expression of mClC-1 in HEK293 cells and skeletal myotubes. An adequate quantitative description of ClC-1 deactivation kinetics requires fitting the deactivation time course with the sum of two exponentials (Warnstedt et al., 2002). Thus, we used a biexponential fitting paradigm to extract the steady-state amplitudes (A_{fast} , A_{slow} , and C) and corresponding deactivation time constants (τ_{fast} and τ_{slow}) that comprise the macroscopic current decay. Fig. 3 depicts the voltage dependence of the relative proportion of slow (A), fast (B), and nondeactivating (C) amplitudes of the total current and the two time constants of deactivation (D) for mClC-1-expressing HEK293 cells (squares), mClC-1-expressing myotubes (triangles), and native wild-type FDB fibers (circles). The fast, slow, and nondeactivating components of mClC-1 exhibit similar voltage dependence in HEK293 cells, myotubes, and FDB fibers and are also similar to that observed for human ClC-1 (Warnstedt et al., 2002). However, across most voltages, the relative amplitude of the slow component in mClC-1-expressing HEK293 cells is significantly ($P < 0.05$) reduced and the fast component increased compared with mClC-1-expressing myotubes and native FDB fibers. In addition, the fast time constant of channel deactivation was also faster in mClC-1-expressing HEK293 cells over the majority of test potentials compared with that observed in native FDB fibers. Thus, an increase in the relative proportion of fast gating and a decrease in the fast time constant of channel deactivation account for the increase in the rate of macroscopic mClC-1 deactivation observed in mClC-1-expressing HEK293 cells.

Together, results presented in Figs. 1–3 provide strong evidence regarding the feasibility of obtaining reliable measures of macroscopic ClC-1 function in FDB fibers obtained from young mice.

Comparison of ClC-1 Properties in FDB Fibers Obtained from Wild-Type and HSA^{LR} Mice

A second aim of this study was to determine if increased muscle hyperexcitability and myotonia observed in HSA^{LR} (Mankodi et al., 2000) and $Mbnl1^{\Delta E3/\Delta E3}$ (Kanadia et al., 2003) mice arises from defects in endogenous ClC-1 channel activity. Fig. 4 depicts representative 9AC-sensitive ClC-1 currents recorded from FDB fibers obtained 18-d-old wild-type (Fig. 4 A) and HSA^{LR} (Fig. 4 B) mice. Average ClC-1 current density measured from 18–20-d-old HSA^{LR} FDB fibers exhibited all of the hallmarks of classic ClC-1 currents, including prominent inward rectification of the instantaneous current with a reversal potential near E_{Cl} (Fig. 4 C), a weak voltage dependence to $P_{O_{rel}}$ (Fig. 4 D), and rapid and voltage-dependent channel deactivation similar to that observed in wild-type FDB fibers (Fig. 5). The most obvious difference observed in HSA^{LR} FDB fibers was a dramatic reduction in ClC-1 current magnitude compared with age-matched wild-type FDB fibers. The reduction in ClC-1 current magnitude was not due to differences in cell size since total membrane capacitance was not significantly different in FDB fibers obtained from 18–20-d wild-type and HSA^{LR} mice (Table I). Peak ClC-1 current density (measured at -140 mV) was reduced $\sim 70\%$ in FDB fibers obtained from 18–20-d-old HSA^{LR} mice (-49.8 ± 3.7 pA/pF, $n = 8$, and -14.0 ± 1.6 pA/pF,

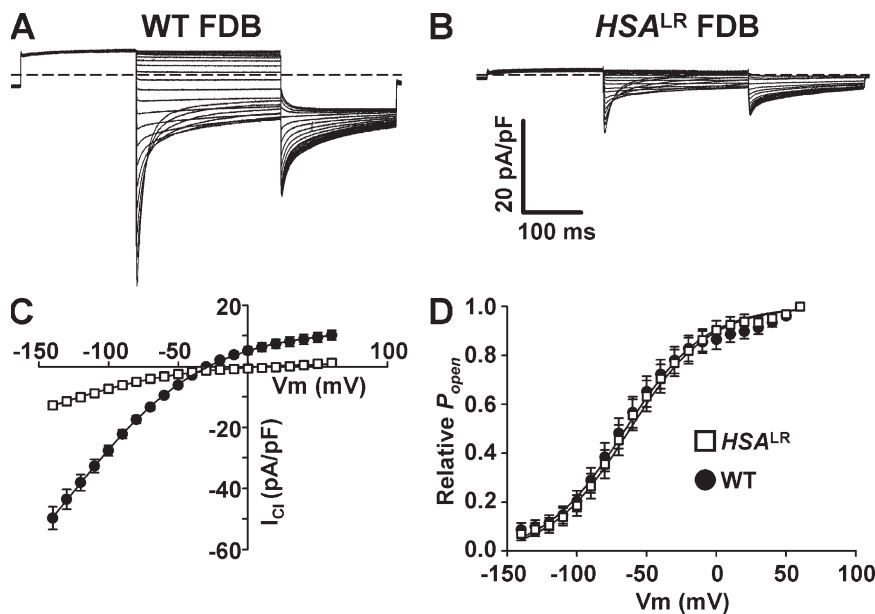


Figure 4. Macroscopic CIC-1 current density is dramatically reduced in FDB fibers of *HSA^{LR}* mice. Representative family of CIC-1 currents recorded from FDB fibers of 19-d-old WT (A) and *HSA^{LR}* (B) mice elicited using an identical voltage protocol (see Fig. 1, top). The dashed lines represent the zero current level. (C) Voltage dependence of average instantaneous current–voltage relationship in FDB fibers obtained from 18–20-d-old WT (closed circles; $n = 8$) and *HSA^{LR}* (open squares; $n = 16$) mice. The apparent depolarizing shift in the reversal potential of the instantaneous CIC-1 current in FDB fibers from *HSA^{LR}* mice most likely arises from difficulty in resolving the true reversal potential in face of small, nearly undetectable, outward currents in these fibers. (D) Average relative P_{σ} - V curves for FDB fibers obtained from 18–20-d-old WT (closed circles; $n = 8$) and *HSA^{LR}* (open squares; $n = 16$) mice. Smooth curves through each P_{σ} - V dataset were generated using a modified Boltzmann equation (Eq. 3).

$n = 15$, for wild-type and *HSA^{LR}* fibers, respectively). Maximal inward steady-state current density was also decreased to a similar degree (unpublished data). Additionally, the reduction in peak CIC-1 current density could not be attributed to a hyperpolarizing shift in the voltage dependence of channel activation (as occurs for certain CIC-1 mutations in dominant myotonia congenita) (Warnstedt et al., 2002), since the voltage dependence of $P_{\sigma_{rel}}$ was not significantly different for FDB fibers obtained from 18–20-d-old wild-type (filled circles) and *HSA^{LR}* (open squares) mice (Fig. 4 D and Table I).

Kinetic Analysis of CIC-1 Deactivation in FDB Fibers from Wild-Type and *HSA^{LR}* Mice

Berg et al. (2004) found that two of the CIC-1 splice variants that commonly occur in DM1 produce both a dominant-negative reduction in wild-type CIC-1 currents and an acceleration in channel deactivation. Therefore, we tested if a similar alteration in CIC-1 deactivation kinetics is also observed in the *HSA^{LR}* mouse model of DM1 by comparing the kinetic parameters of CIC-1 channel deactivation in FDB fibers obtained from 18–20-d-old wild-type and *HSA^{LR}* mice. Normalization of channel deactivation in wild-type and *HSA^{LR}* fibers reveals that the deactivation time course at -100 mV is indeed faster in *HSA^{LR}* fibers (Fig. 5 A left, dashed lines). Nevertheless, a quantitative description of the time course of CIC-1 deactivation still requires the sum of two exponential functions in both wild-type and *HSA^{LR}* FDB fibers. The biexponential nature of channel deactivation is best appreciated by replotting the currents from wild-type (Fig. 5 A, middle) and

HSA^{LR} (Fig. 5 A, right) fibers on a semilogarithmic scale. In this analysis, the steady-state amplitudes of the slow (A_{slow}), fast (A_{fast}), and nondeactivating (C) components are represented by their respective Y intercepts. The voltage dependence of the relative contributions of A_{slow} (A_{slow}/A_{total} ; where $A_{total} = A_{slow} + A_{fast} + C$), A_{fast} (A_{fast}/A_{total}), and C (C/A_{total}) to channel deactivation and the magnitude of the two deactivation time constants (τ_{slow} and τ_{fast}) are summarized in Fig. 5 (B–E, respectively). The results show that a significant acceleration in channel deactivation observed at intermediate voltages (-80 to -120 mV) in *HSA^{LR}* FDB fibers arises from an increase in the fractional contribution of the fast component of channel deactivation coupled with a parallel decrease in the relative contribution of the slow component of channel deactivation. Specifically, CIC-1 channels in *HSA^{LR}* FDB fibers exhibit a significant increase in fast gating by up to $\sim 15\%$ at -100 mV without a significant effect on the relative contribution of the nondeactivating component. On the other hand, the time constants of channel deactivation (τ_{slow} and τ_{fast}) were not different across these intermediate voltages, although τ_{fast} was somewhat reduced at very negative potentials in *HSA^{LR}* fibers. These data indicate that faster channel deactivation in *HSA^{LR}* fibers at intermediate voltages arises from an increase in the relative contribution of the fast gating component of channel deactivation.

Kinetic Analysis after Prepulse-dependent Reduction in CIC-1 Cl^{-} Current Density in Wild-Type FDB Fibers

The increase in the contribution of the fast component of channel deactivation could arise either from

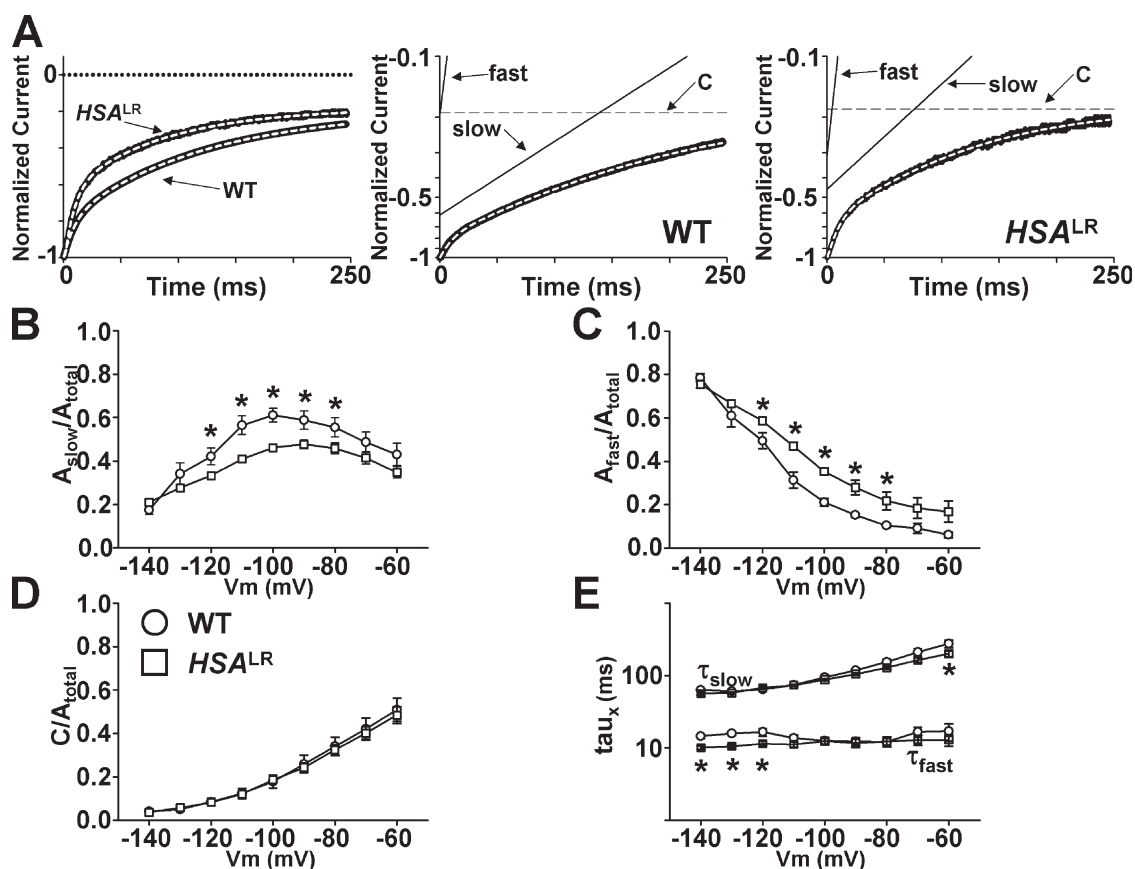


Figure 5. Deactivation kinetics of ClC-1 currents in FDB fibers obtained from WT and *HSA^{LR}* mice. (A) Superimposed traces of normalized ClC-1 current deactivation (solid lines) elicited at -100 mV in FDB fibers obtained from 19-d-old WT and *HSA^{LR}* mice and fit with a second order exponential (left; white dashed lines). ClC-1 currents from representative WT (middle) and *HSA^{LR}* (right) FDB fibers fit with a biexponential function and replotted on log-linear plots. Fractional amplitudes of the extracted slow, fast, and nondeactivating components of the currents are shown for clarity. (B–D) Voltage dependence of the average relative contribution of the slow (B), fast (C), and steady-state (D) components of ClC-1 deactivation in FDB fibers obtained from 18–20-d-old WT (open circles, $n = 8$) and *HSA^{LR}* (open squares, $n = 16$) mice. (E) Voltage dependence of the fast and slow time constants of ClC-1 deactivation in FDB fibers obtained from 18–20-d-old WT (open circles, $n = 8$) and *HSA^{LR}* (open squares, $n = 16$) mice. *, $P \leq 0.05$.

dominant-negative effects on channel gating of novel splice isoforms present in *HSA^{LR}* fibers (Berg et al., 2004) or as a result of the dramatically different ClC-1 current magnitudes found in wild-type and *HSA^{LR}* fibers. To test the latter, we quantified ClC-1 deactivation at -100 mV in 18–20-d-old wild-type FDB fibers after 200-ms prepulses to potentials ranging from $+60$ mV to -80 mV (10-mV increments). Using this approach, we were able to compare the kinetics of ClC-1 deactivation during a single test pulse (-100 mV) across a broad range of different ClC-1 current densities within the same cell. Fig. 6 A shows a family of ClC-1 test pulse currents obtained from a 19-d-old wild-type FDB fiber. The prepulse dependence of the time-dependent ClC-1 current (i.e., the A_{fast} and A_{slow} components) during the test pulse is shown in Fig. 6 B. Superimposing the largest ClC-1 current (using a $+60$ mV prepulse) with the normalized current after a 50% reduction in open probability (using a -70 -mV prepulse) reveals that the deactivation time course is essentially identical for the two markedly

different ClC-1 currents (Fig. 6 B, inset). In fact, prepulse-dependent changes in ClC-1 current magnitude did not significantly affect the relative contribution of the fast and slow gating component of deactivation or their respective time constants (Fig. 6 C). The relative contributions of the fast and slow components of channel deactivation (at -100 mV) and the values of their respective time constants in WT ($+60$ mV prepulse), 50% reduced WT (-70 mV prepulse), *HSA^{LR}* ($+60$ mV prepulse), and *Mbn1^{ΔE3/ΔE3}* ($+60$ mV prepulse) are compared in Fig. 6 D. These results indicate that faster kinetics of deactivation observed in *HSA^{LR}* and *Mbn1^{ΔE3/ΔE3}* does not result from a current-dependent effect on channel gating.

Nonstationary Noise Analysis in FDB Fibers from Wild-Type, *HSA^{LR}*, and *Mbn1^{ΔE3/ΔE3}* Mice

The absence of a significant difference in the voltage dependence of P_{open} between FDB fibers obtained from wild-type and *HSA^{LR}* mice indicates that the observed

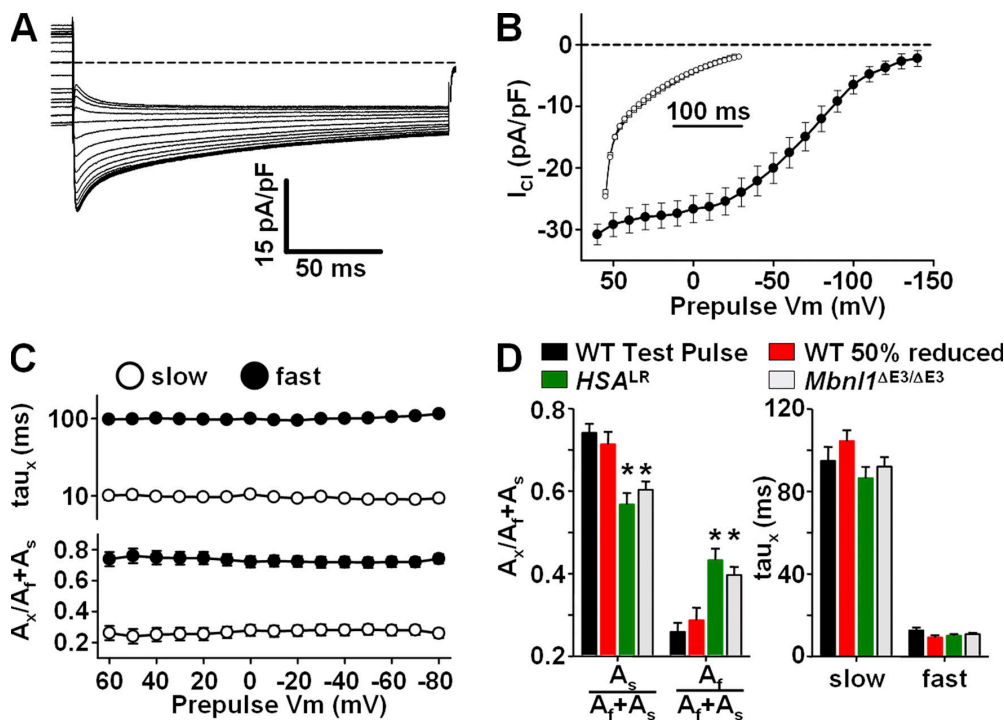


Figure 6. Kinetics of CIC-1 deactivation after prepulse-dependent current reduction. (A) Representative family of CIC-1 currents (at -100 mV) recorded from an FDB fiber obtained from a 19-d-old WT mouse after 200-ms prepulses to potentials ranging from $+60$ to -140 mV (in 10-mV increments). (B) Voltage dependence of average time-dependent currents ($A_{fast}+A_{slow}$) after prepulse-dependent current reduction. (Inset) Normalized CIC-1 currents (solid lines) fit with a second order exponential in control (60 mV prepulse; circles) and after $\sim 50\%$ (average = $48.8 \pm 0.1\%$, $n = 8$) reduction in current magnitude (-70 mV prepulse; squares). Black dashed line indicates the zero current level. (C, bottom) Voltage dependence of the average relative contribution

of the fast (closed circles) and slow (open circles) components of CIC-1 deactivation (C, lower) and their respective time constants (C, top). (D) Average relative contribution of the fast and slow components of the time-dependent current ($A_{fast}+A_{slow}$) and their respective time constants to CIC-1 deactivation (at -100 mV) in FDB fibers obtained from WT mice ($+60$ mV prepulse; black, $n = 8$), WT mice after $\sim 50\%$ reduction in CIC-1 current magnitude (-70 mV prepulse; red, $n = 8$), HSA^{LR} mice ($+60$ mV prepulse; green, $n = 14$), $Mbn11^{\Delta E3/\Delta E3}$ mice ($+60$ mV prepulse; white; $n = 11$). *, $P \leq 0.05$ compared with WT $+60$ mV prepulse.

reduction in CIC-1 current density in HSA^{LR} fibers must result from a reduction in the number of functional channels (N), single channel conductance (γ), and/or maximal channel open probability ($P_{o_{max}}$). To determine which of these parameters account for the $\sim 70\%$ reduction in CIC-1 current density in HSA^{LR} fibers, non-stationary noise analysis was performed from whole-cell patch clamp measurements of CIC-1 channel activity in FDB fibers of 12-d-old wild-type and 18–21-d-old HSA^{LR} mice (Fig. 7). Fig. 7 A shows representative mean 9AC-sensitive CIC-1 currents recorded from 92 and 79 consecutive 200-ms voltage steps to -140 mV after a 200-ms prepulse at $+60$ mV from FDB fibers obtained from a 12-d-old wild-type (left) and a 19-d-old HSA^{LR} (right) mouse, respectively. The corresponding time course of the current variance for each experiment is shown in Fig. 7 B and the mean–variance relationships are plotted in Fig. 7 C. The mean–variance plots were fitted according to Eq. 4 in order to extract the values of i , N , and $P_{o_{max}}$ (the latter from Eq. 5). Average values for i , γ , and $P_{o_{max}}$ obtained from native FDB fibers using this approach (Table II) are similar to those reported previously after heterologous expression of hCIC-1 in tSA201 (Hebeisen et al., 2004), *Xenopus* oocytes (Rychkov et al., 1998), and HEK 293 cells (Pusch et al., 1994; Rosenbohm et al., 1999). We found that single channel CIC-1 cur-

rent amplitude (0.25 ± 0.03 pA and 0.30 ± 0.03 pA, respectively) and conductance (2.3 ± 0.02 pS and 2.8 ± 0.03 pS, respectively) were not significantly different between FDB fibers obtained from wild-type and HSA^{LR} mice. A small, but significant ($P < 0.01$), reduction in maximum channel open probability was observed in HSA^{LR} FDB fibers (0.91 ± 0.01 and 0.75 ± 0.03 for wild-type and HSA^{LR} fibers, respectively). However, the major effect observed was a dramatic reduction (65%) in CIC-1 channel density HSA^{LR} fibers (170 ± 21 and 58 ± 11 channels/pF for wild-type and HSA^{LR} fibers, respectively), which was primarily responsible for the $\sim 70\%$ reduction in CIC-1 current density (-37.8 ± 2.6 and -12.0 ± 1.4 pA/pF for wild-type and HSA^{LR} fibers, respectively) observed in these experiments. Since there is an approximately twofold increase in macroscopic CIC-1 current density between postnatal day 12 and day 18 in HSA^{LR} mice (unpublished data), the observed reduction in peak I_{Cl} reported in Table II likely reflects a lower estimate of the decrease in CIC-1 activity. Qualitatively similar effects on CIC-1 channel magnitude (Fig. 8, A and B), voltage dependence of $P_{o_{rel}}$ (Fig. 8 C), deactivation kinetics (Fig. 6 D, white bars), and single channel properties assessed from nonstationary noise analysis (Fig. 8, D and E; Table II) were observed in experiments conducted in 12-d-old wild-type control and $Mbn11$

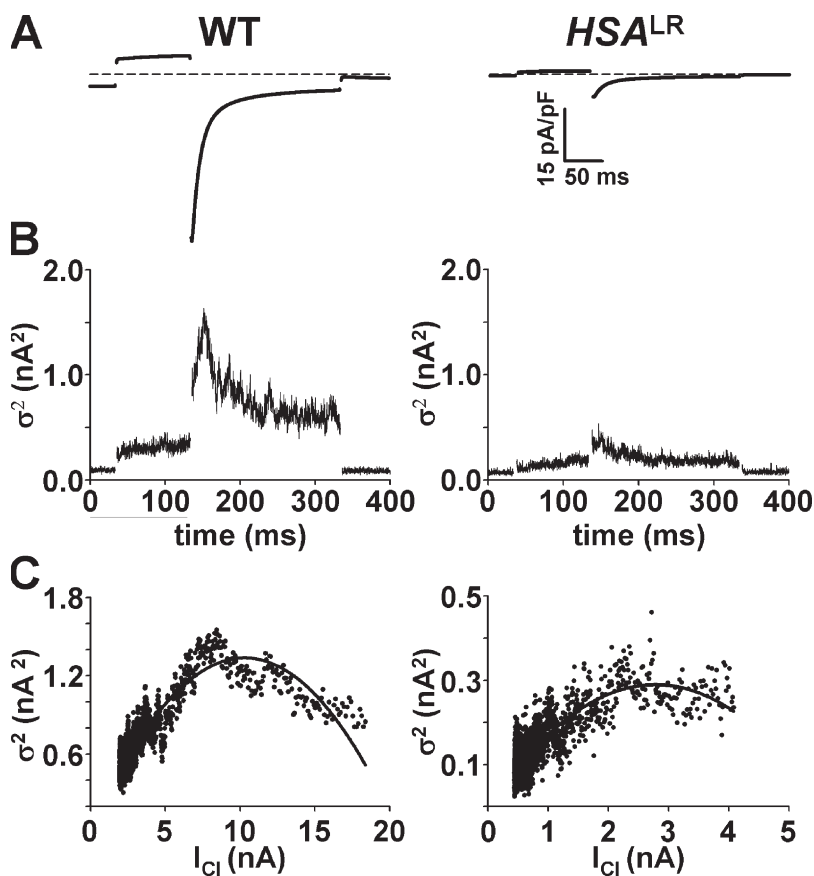


Figure 7. Nonstationary noise analysis during ClC-1 deactivation in FDB fibers obtained from wild-type and *HSA^{LR}* mice. (A) Representative mean currents in FDB fibers obtained from 12-d-old WT (left) and 18-d-old *HSA^{LR}* (right) mice elicited using a 200-ms voltage step to -140 mV after a 100-ms prepulse to $+60$ mV. The initial 2 ms of each voltage step is blanked and the total duration of the traces truncated to 400 ms for clarity. (B) Variance time course for the currents shown in A. (C) Mean-variance relationships for the experiments shown in A and fit by Eq. 4 (see Table II for average values of fitted parameters).

knockout (*Mbnl1* ^{$\Delta E3/\Delta E3$}) mice, a second mouse model for DM that exhibits aberrant *Clcn1* splicing and prominent myotonia (Kanadia et al., 2003).

DISCUSSION

The pathogenic mechanism for myotonia in DM has long been debated. Incomplete sodium channel inactivation (Mounsey et al., 2000) and an increase in the activity of small conductance, calcium-activated po-

tassium channels have been suggested to contribute to increased muscle excitability and susceptibility to myotonia in DM (Renaud et al., 1986; Behrens et al., 1994; Kimura et al., 2003). Alternatively, myotonia in DM has also been suggested to arise from a dramatic reduction in transmembrane chloride conductance that results from expanded CUG repeat-containing mRNA molecules sequestering/inactivating MBNL1 proteins required for proper splicing of *CLCN1* pre-mRNA (Mankodi et al., 2002; Kanadia et al., 2003). Our results

TABLE II
Parameters of Nonstationary Noise Analysis

	WT ($n = 8$)	<i>HSA^{LR}</i> ($n = 17$)	<i>Mbnl1</i> ^{+/+} ($n = 5$)	<i>Mbnl1</i> ^{$\Delta E3/\Delta E3$} ($n = 4$)
	12 d	18–21 d	12 d	12 d
Capacitance (pF)	404 \pm 26	722 \pm 29 ^b	596 \pm 46	439 \pm 33 ^a
i (pA)	0.25 \pm 0.03	0.30 \pm 0.03	0.23 \pm 0.04	0.26 \pm 0.04
g (pS)	2.3 \pm 0.02	2.8 \pm 0.03	2.2 \pm 0.04	2.5 \pm 0.04
P_{0max}	0.91 \pm 0.01	0.75 \pm 0.03 ^b	0.86 \pm 0.01	0.76 \pm 0.03 ^b
N	69,165 \pm 9,131	44,868 \pm 9,892	173,908 \pm 32,520	52,387 \pm 9,589 ^b
N/pF	170 \pm 21.0	58 \pm 11.0 ^b	298 \pm 65.0	121 \pm 22.0 ^a
Peak I_{Cl} (pA/pF)	-37.8 \pm 2.6	-12.0 \pm 1.4 ^b	-60.8 \pm 4.4	-23.6 \pm 3.2 ^b

Separate WT controls were conducted for *HSA^{LR}* and *Mbnl1* ^{$\Delta E3/\Delta E3$} because the two mouse lines are on different genetic backgrounds (FVB and C57Bl6, respectively).

^aP < 0.05.

^bP < 0.01.

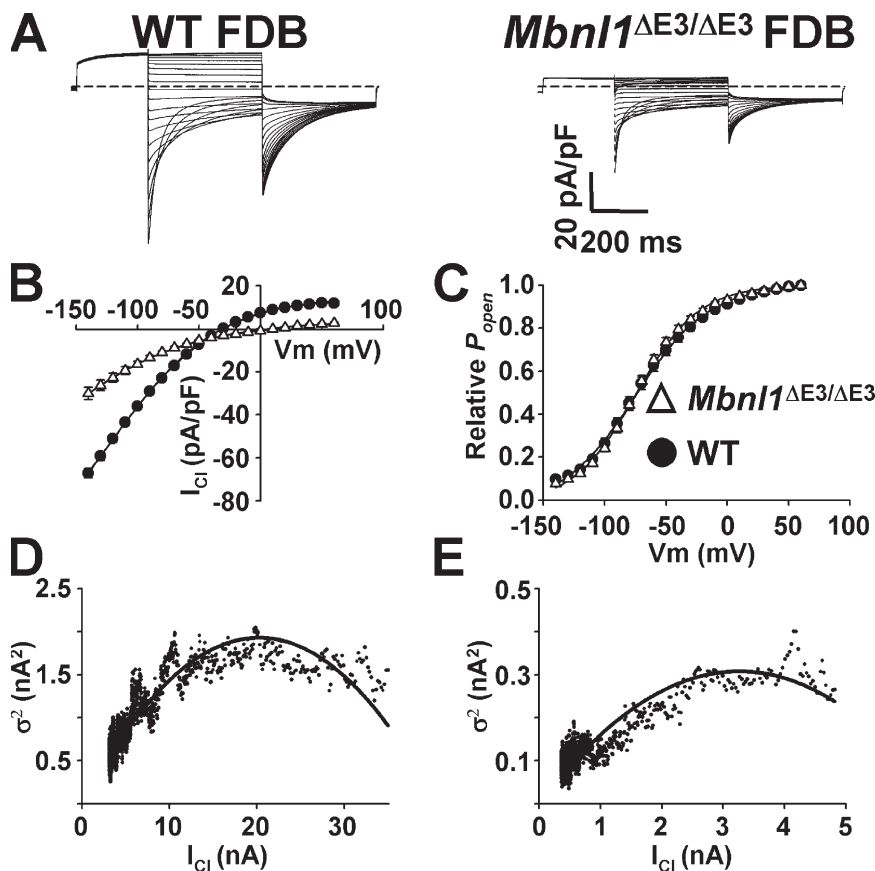


Figure 8. Macroscopic ClC-1 current density is reduced in FDB fibers from *Mbnl1*^{ΔE3/ΔE3} mice. (A) Representative family of ClC-1 currents recorded from FDB fibers obtained from 14-d-old WT (left) and *Mbnl1*^{ΔE3/ΔE3} (right) mice. (B) Average instantaneous ClC-1 current-voltage curves for fibers obtained from 9–14-d-old WT (closed circles, *n* = 22) and *Mbnl1*^{ΔE3/ΔE3} (open triangles, *n* = 16) mice. (C) Average relative *P*_{open}-*V* curves for FDB fibers obtained from 9–14-d-old WT (closed circles) and *Mbnl1*^{ΔE3/ΔE3} (open triangles) mice. Smooth curves through each *P*_σ-*V* dataset were generated using a modified Boltzmann equation (Eq. 3). (D and E) Representative mean-variance relationships for FDB fibers obtained from 12-d-old WT (D) and *Mbnl1*^{ΔE3/ΔE3} (E) mice elicited using a 200-ms voltage step to -140 mV after a 100-ms prepulse to +60 mV (see Table II for average values of fitted parameters).

obtained from two murine models for myotonia in DM1 are consistent with the later mechanism leading to a marked pathogenic reduction in the number of functional ClC-1 channels in the sarcolemma of skeletal muscle. Important novel contributions of this study include (a) the first complete biophysical characterization of ClC-1 function in native skeletal muscle fibers using macroscopic whole-cell and nonstationary noise analysis approaches; (b) functional characterization of a newly cloned murine ClC-1 channel (mClC-1) and demonstration that heterologous expression of mClC-1 in HEK293 cells and homologous expression in skeletal myotubes faithfully reproduces the biophysical properties of ClC-1 measured from native FDB fibers; (c) demonstration that increased muscle excitability in two mouse models of DM (*HSA*^{LR} and *Mbnl1*^{ΔE3/ΔE3} mice) is associated with a severe reduction in sarcolemmal ClC-1 activity stemming primarily from a decrease in the number of functional ClC-1 channels; and (d) evidence for reduced maximum ClC-1 channel open probability and accelerated kinetics of channel deactivation in FDB fibers of *HSA*^{LR} and *Mbnl1*^{ΔE3/ΔE3} mice. Together, these results provide strong support for the toxic RNA model for DM pathogenesis in which myotonia results from a transdominant effect of CUG repeat-containing mRNA on MBNL1-mediated control of proper splicing of *CLCN1* pre-mRNA.

Biophysical Characterization of ClC-1 Channel Function in Native FDB Fibers

Macroscopic ClC-1 channel activity in skeletal muscle has previously been measured using double sucrose (Duval and Leoty, 1980), vaseline gap (Fahlke and Rudel, 1995), and two-electrode (Chen and Jockusch, 1999) voltage clamp techniques. However, under certain conditions, whole-cell patch clamp experiments can afford superior control over the intracellular environment, blockade of overlapping ionic currents, and provide enhanced voltage clamp speed and uniformity. Unfortunately, whole-cell voltage clamp measurements of ClC-1 channel activity have only been previously reported after heterologous expression of cloned ClC-1 channels (Steinmeyer et al., 1991; Pusch et al., 1994; Warnstedt et al., 2002). Here we report the first complete biophysical characterization of the voltage dependence and kinetics of ClC-1 channel activity using whole-cell voltage clamp and nonstationary noise analysis approaches in native skeletal muscle fibers. In our experiments, ClC-1 currents were carefully isolated by eliminating sodium (0 extracellular sodium), potassium (0 extracellular potassium, extracellular TEA, and intracellular cesium), and calcium (3 μM nifedipine) currents. In addition, for all experiments, leak and capacitive currents were removed by offline subtraction of 9AC-insensitive currents. The resulting 9AC-sensitive currents exhibited all

of the hallmarks of ClC-1 currents observed for heterologously (e.g., *Xenopus* oocytes, Sf9 cells, COS-7 cells, HEK293 cells) expressed cloned ClC-1 channels (Figs. 1–3). Specifically, similar to heterologously expressed ClC-1 channels, ClC-1 currents in native FDB fibers exhibited chloride selectivity (E_{rev} being close to E_{Cl}) and instantaneous and steady-state current–voltage relationships with characteristic inward rectification and “S”-shaped voltage dependence, respectively (Fig. 2, A–D). Moreover, relative P_o –voltage relationships based on normalized isochronal measurements of tail current amplitudes exhibited sigmoidal voltage dependence with similar slope and $V_{1/2}$ values (Fig. 2 E and Table I). Finally, ClC-1 current deactivation in native FDB fibers and mClC-1–expressing myotubes and HEK293 cells were all well described by a biexponential function (Fig. 3). These results demonstrate the reliability of our biophysical characterization of ClC-1 activity in native FDB fibers.

Coonan and Lamb (1998) suggested that a second chloride channel (insensitive to extracellular 9AC) may contribute to the total chloride conductance in rat skeletal muscle. Our results in which 1 mM 9AC rapidly blocked 98% of all chloride conductance under our recording conditions (Fig. 1, right), argues against a significant contribution of 9AC-insensitive chloride channels in mouse FDB fibers. However, we cannot rule out a potential role of calcium-activated chloride channels that would likely be inhibited/blocked under our recording conditions (i.e., in the presence of 10 mM intracellular EGTA).

Influence of Cellular Context on ClC-1 Activity

We carefully compared the biophysical properties (voltage dependence of instantaneous, steady-state, $P_{o,reb}$ and kinetics of channel deactivation) of ClC-1 channel activity in native murine FDB fibers with that of mClC1 expressed in both HEK293 cells and primary cultures of skeletal myotubes. To our knowledge, this study is the first to provide a comprehensive, side-by-side comparison of the functional properties of exogenously expressed mClC-1 channels to that of native ClC-1 currents. We compared murine ClC-1 channel properties under three separate cellular contexts (native FDB fibers and mClC-1 expressed in HEK293 cells and primary mouse myotubes). Not surprisingly the macroscopic properties of mClC-1 expressed in HEK293 cells reported here are nearly identical to those previously reported for heterologous expression of cloned human (87% identical) and rat (96% identical) ClC-1 recorded under similar conditions (Rychkov et al., 1998). We also characterized mClC-1 properties after homologous expression in primary skeletal myotubes since myotubes represent an early developmental state of muscle that lacks endogenous ClC-1 channel expression (Fig. 2 B, upright triangles) (Conte Camerino

et al., 1989; Wischmeyer et al., 1993; Bardouille et al., 1996). Thus, comparing mClC-1 properties after heterologous expression in HEK293 cells with that observed in native FDB fibers and after homologous expression in myotubes could reveal potential “muscle-specific” modulatory effects on ClC-1 function that may not be faithfully reproduced using standard heterologous expression systems (e.g., HEK293 cells). Overall, ClC-1 functional properties (e.g., reversal potential, inward rectification of the instantaneous I-V relationship, voltage dependence of steady-state activation and $P_{o,reb}$ deactivation kinetics) were remarkably similar in HEK293 cells, myotubes, and native FDB fibers (Figs. 1–3). However, we found that the relative rate of ClC-1 channel deactivation across most voltages was significantly slower in FDB fibers and mClC-1–expressing myotubes (Fig. 3). Thus, it is possible that muscle-specific regulatory mechanisms absent in HEK293 cells may influence ClC-1 gating. Nevertheless, the overall similarity of ClC-1 biophysical properties in native murine FDB fibers and mClC-1–expressing myotubes and HEK293 cells indicates that basal ClC-1 function is not markedly influenced by cellular context and provides strong justification for the evaluation of mClC-1 function using heterologous expression systems.

Previous work indicates that ClC-1 transcription in native tissue is strongly dependent on muscle electrical activity. During muscle denervation, there is a rapid decrease in the levels of ClC-1 transcript in parallel with a reduction in ClC-1 channel activity (Conte Camerino et al., 1989; Klocke et al., 1994; Chen and Jockusch, 1999). Papponen et al. (2005) used antibodies raised against the C terminus of ClC-1 to suggest that ClC-1 protein is not detectable in the sarcolemma of freshly dissociated FDB fibers. This study also found that overnight incubation with staurosporin was required for reinsertion of ClC-1 channels into the sarcolemma. Additionally, a recombinant Semliki Forest virus was used to express myc-tagged ClC-1 proteins in myoblasts and myotubes derived from rat L6 myogenic cells. Surprisingly, ClC-1 proteins were found to be localized to unidentified intracellular vesicles and not in the sarcolemma after expression in L6 myoblasts and myotubes (Papponen et al., 2005). However, in these studies, sarcolemmal ClC-1 expression was only assessed using imaging approaches and was not corroborated using electrophysiology recordings of transmembrane ClC-1 currents. Under our experimental conditions, we were able to measure robust ClC-1 channel activity in both freshly dissociated FDB fibers and after nuclear injection of mClC-1 cDNA in primary mouse skeletal myotubes. Since our experiments provide no measure of ClC-1 channel activity before fiber isolation, significant ClC-1 internalization during dissociation is possible. However, we observed no significant time-dependent decrease in ClC-1 current density up to 8 h after fiber

isolation and only a 16% decrease >24 h after isolation (unpublished data).

Role of CIC-1 Channel Dysfunction in Two Mouse Models of Myotonic Dystrophy

Transmembrane chloride conductance (G_{Cl}) comprises 70–80% of the total resting membrane conductance in mammalian skeletal muscle, the remainder of which results from background potassium channels (Rudel and Lehmann-Horn, 1985). This large G_{Cl} acts to stabilize the resting membrane potential. During activation of skeletal muscle, action potentials rapidly propagate deep into the muscle fiber along the transverse tubule (t-tubule) membrane system. The extensive t-tubule invaginations create a diffusion-limited space that can result in significant potassium accumulation during trains of muscle excitation (Neelands et al., 2001). In the absence of a large G_{Cl} , this potassium accumulation depolarizes the membrane potential and promotes muscle excitability. Thus, CIC-1 channels in skeletal muscle provide a critical short-circuit current that acts to counteract the excitatory influence of excessive potassium accumulation within the t-tubule system. Reduction of G_{Cl} by >50% is sufficient to promote myotonia in both humans and experimental animals (Bryant and Morales-Aguilera, 1971; Rudel and Lehmann-Horn, 1985), as demonstrated through partial CIC-1 current blockade using aromatic monocarboxylic acid channel blockers (Furman and Barchi, 1978). Moreover, mutations in *CLCN1* result in both dominant and recessive myotonia congenita (Pusch, 2002). Dominant mutations in CIC-1 typically produce a depolarizing shift in the voltage dependence of CIC-1 activation, which results in a decrease in CIC-1 open probability at the resting membrane potential, and consequently an increased susceptibility to myotonia in goats (Beck et al., 1996) and humans (Rudel et al., 1988). In general, recessive mutations result in nonfunctional channels and an elimination of sarcolemmal CIC-1 conductance. However, DM has not been linked to mutations in *CLCN1* or any other ion channel gene.

Our results indicate that macroscopic CIC-1 current density (measured at -140 mV) was reduced 70% and 61% in freshly dissociated FDB fibers isolated from 18–20-d-old *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* (Figs. 4 and 8) mice, respectively. This reduction in CIC-1 function may actually be an underestimate of the effect observed at physiologic potentials since a greater degree of inward rectification was observed for CIC-1 currents recorded from FDB fibers of *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* mice (Fig. 4 C and Fig. 8 B). Nonstationary noise analysis revealed that this reduction in macroscopic CIC-1 current density arises from a marked decrease in number of functional channels and a minor decrease (16%) in $P_{O_{max}}$ (Table II). However, since the small reduction in $P_{O_{max}}$ occurred in the absence of a significant shift in the voltage dependence of the $P_{O_{rel}}$ (Fig. 4 D and Fig. 8 C), a de-

crease in $P_{O_{max}}$ can only contribute minimally to the observed reduction in macroscopic CIC-1 current. In addition, no change in single channel conductance (γ) was observed in FDB fiber obtained from *HSA^{LR}* or *Mbnl1^{ΔE3/ΔE3}* mice. Rather, the observed reduction in macroscopic CIC-1 current density in *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* fibers resulted primarily from a reduction in CIC-1 channel density in both animal models (Table II). This reduction in the number of functional CIC-1 channels could arise from a decrease in the amount of full-length CIC-1 protein, dominant-negative effects of truncated isoforms on the full-length protein (Berg et al., 2004), or a combination of both. Distinguishing between the relative impact of these potential mechanisms will require determining the expression levels of full-length and truncated CIC-1 proteins and also assessing the effects of truncated isoforms on full-length protein expression, stability, and function.

Although CIC-1 currents in FDB fibers obtained from *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* mice exhibited very similar properties to those observed for wild-type fibers, CIC-1 currents from the animal models deactivated significantly faster than wild-type fibers. This difference in the rate of channel deactivation resulted from parallel shifts in the relative proportion of the fast and slow components of channel deactivation with minimal effects on the time constants of each component. Aberrant splicing of *Cln1* pre-mRNA leads to the production of truncated transcripts (Mankodi et al., 2002), that have been shown to both lower CIC-1 current density and modify the rate of channel deactivation (Berg et al., 2004). The most prominent aberrant splice product ($44 \pm 3\%$) identified in *HSA^{LR}* muscle results from the inclusion of an additional exon cassette between exons 6 and 7 (named exon 7a), which leads to the introduction of a premature stop codon (Mankodi et al., 2002). A similar splice product, which includes two additional exon cassettes 6b and 7a, is expressed in human DM1 muscle. The DM1 (exon 6b/7a⁺) and *HSA^{LR}* (exon 7a⁺) variants are truncated at similar positions (codon 283 in DM1, codon 290 in *HSA^{LR}*). Recently, Berg et al. (2004) found that coinjection of *Xenopus* oocytes with the 283x (exon 6b/7a⁺) splice variant results in a significant reduction in wild-type hCIC-1 current density and an acceleration in channel deactivation. Thus, our findings of a small, but significant, reduction in CIC-1 $P_{O_{max}}$ observed in nonstationary noise analysis experiments (Table II) and accelerated channel deactivation are consistent with the results of Berg et al. (2004) and support the conclusion that truncated CIC-1 protein products exert a dominant-negative effect on full-length CIC-1 channels in DM1 muscle. In addition, the observed reduction in the number of functional CIC-1 channels might also result from dominant-negative effects of truncated fragments on CIC-1 trafficking, degradation, or function. Together our observation of decreased $P_{O_{max}}$ and accelerated deactivation

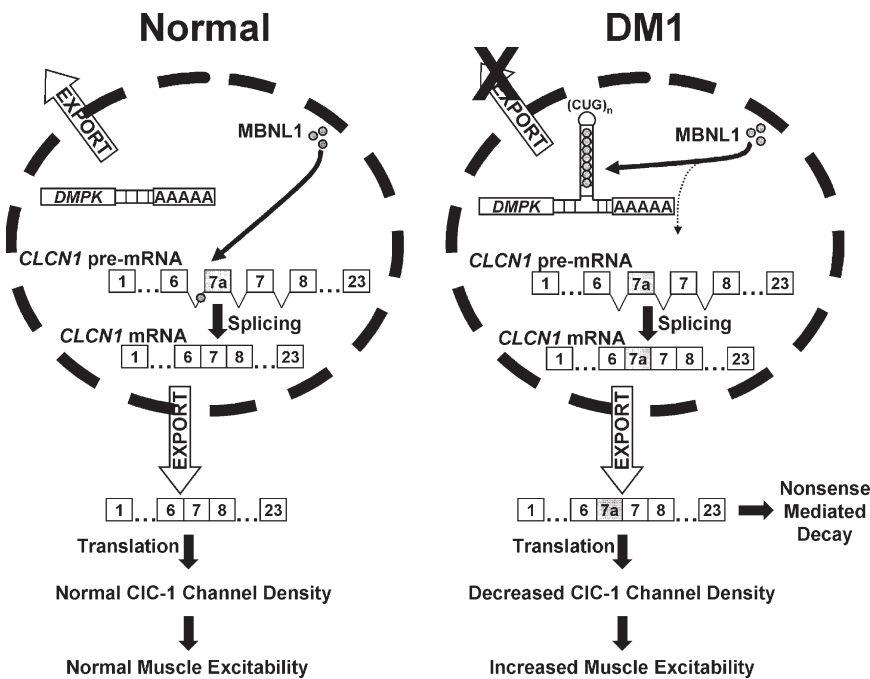


Figure 9. Proposed molecular model for increased muscle excitability in DM1. (Left) Proper *CLCN1* pre-mRNA splicing in normal skeletal muscle is regulated by muscleblind-like 1 (MBNL1) proteins, which are shown to bind to hypothetical intronic splice repressor elements in intron 6. (Right) Altered *CLCN1* pre-mRNA splicing in DM1 arises from *DMPK* transcripts with expanded repeats (CUG)_n accumulating in nuclear foci and sequestering double-stranded CUG binding proteins, including MBNL1. Depletion of MBNL1 proteins results in inclusion of additional exons (e.g., exon 7a) containing premature termination codons. Additionally, aberrantly spliced *CLCN1* transcripts are subsequently exported from the nucleus, degraded through the nonsense-mediated decay pathway, and/or produce truncated proteins that potentially exert additional dominant-negative effects on CIC-1 function (Berg et al., 2004). These effects result in a dramatic reduction in the number of functional CIC-1 channels and a subsequent increase in muscle excitability.

kinetics in FDB fibers from *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* mice coupled with the heterologous expression studies of Berg et al. (2004) suggest that truncated CIC-1 fragments exert dominant-negative effects on CIC-1 channel activity.

Molecular Mechanism for a Pathogenic Reduction in Functional CIC-1 Channel Density in DM1

The role of altered CIC-1 function in mediating the myotonic phenotype of DM1 has long been debated. No mutations in the *CLCN1* gene have been identified in DM1 patients, indicating that any effect on CIC-1 function is likely to be indirect. In this study, we found that the number of functional CIC-1 channels in FDB fibers of *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* mice is reduced to levels sufficient to account for an increased susceptibility to myotonia. Although effects of truncated fragments on functional CIC-1 channel trafficking/degradation cannot be ruled out (see above), the observed reduction in functional CIC-1 channel density (66%) in *HSA^{LR}* fibers correlates well with the incidence of aberrant *Cln1* pre-mRNA splicing (76%). This supports the idea that the reduction in the number of functional CIC-1 channels primarily reflects a reduction in the level of *Cln1* mRNA that encodes full-length channels (Mankodi et al., 2002). Thus, a major fraction of the reduction in the number of functional CIC-1 channels likely results from a post-transcriptional effect. In any event, the observed reduction in number of functional CIC-1 channels in FDB fibers of *HSA^{LR}* and *Mbnl1^{ΔE3/ΔE3}* mice is sufficient to account for the prominent myotonia observed in these two murine models of DM.

A central question is how do transcripts containing expanded CUG repeats and MBNL1 deficiency both lead to a similar reduction in *Cln1* mRNA, and subsequently, a parallel decrease in the number of functional CIC-1 channels? One potential mechanism is outlined by the molecular model shown in Fig. 9. This model, which is derived from both prior published reports and the functional results presented in this study, illustrates how proper pre-mRNA splicing of *Cln1* transcripts and subsequent production of sufficient CIC-1 channel activity leads to protection from myotonia in wild-type skeletal muscle (Fig. 9, left) and how this process might be disrupted in DM1 (Fig. 9, right). In normal muscle, MBNL1 proteins translocate to the nucleus and direct proper splicing of a subset of genes that includes *CLCN1*. Proper excision of introns from *CLCN1* pre-mRNA results in the generation of full-length transcripts that are exported from the nucleus and used to produce functional CIC-1 homodimeric channels. In DM1, a CTG repeat expansion in the 3' untranslated region of the *DMPK* gene results in the production of mRNA species that contain several hundred to several thousand CUG repeats. The expanded CUG repeats form a secondary hairpin structure that is recognized by MBNL1, a regulator of alternative splicing. The CUG-MBNL1 complex is retained in the nucleus in discrete foci because the amount of expanded CUG repeat RNA is sufficient to sequester MBNL1 protein. The resulting MBNL1 deficiency leads to aberrant splicing of *Cln1* pre-mRNA and inclusion of additional exons that introduce premature stop codons; the predominant splice defect involves inclusion of a portion of intron

7 (termed exon7a). Some of the resulting aberrantly spliced transcripts are degraded through the nonsense-mediated decay pathway while others are exported and direct the translation of nonfunctional truncated ClC-1 protein products. This results not only in a dramatic reduction in the number of functional full-length ClC-1 channels, but also in the accumulation of truncated fragments that potentially exert dominant-negative effects on full-length ClC-1 channel current magnitude (Berg et al., 2004), deactivation kinetics (Berg et al., 2004; Fig. 5 and Fig. 6 D), and maximum channel open probability (Table II). Together, these effects result in a large reduction in transmembrane ClC-1 channel activity, and therefore increased susceptibility to myotonia due to the loss of an essential short-circuit current required to counteract the excitatory influence of potassium accumulation in the t-tubule system during muscle excitation.

The model depicted in Fig. 9 explains results of this study obtained using two murine models for myotonia in DM1. First, the decrease in the number of functional ClC-1 channels in *HSA^{LR}* mice likely results from aberrant splicing of *Clcn1* pre-mRNA caused by muscle-specific expression of expanded CUG repeat-containing mRNA species that bind/sequester Mbn1l proteins. Loss of Mbn1l-mediated regulation of proper *Clcn1* splicing leads to a severe reduction in the level of full-length *Clcn1* mRNA and the production of aberrantly spliced *Clcn1* transcripts that encode truncated protein products that may exert additional dominant-negative effects on ClC-1 function; effects that together lead to a subsequent pathogenic reduction in ClC-1 current density. A similar cascade of events would also be expected to occur during Mbn1l deficiency in skeletal muscle of *Mbn1l^{ΔE3/ΔE3}* mice. Important implications of this pathogenic mechanism are that exogenous delivery of either wild-type ClC-1 channels or Mbn1l proteins might prove effective in rescuing myotonia in *HSA^{LR}* and *Mbn1l^{ΔE3/ΔE3}* mice (Kanadia et al., 2006) and, if so, would provide a “proof of concept” for ClC-1 and/or *Mbn1l* gene therapeutic approaches for the treatment of myotonia in DM.

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